



저작자표시-비영리-변경금지 2.0 대한민국

이용자는 아래의 조건을 따르는 경우에 한하여 자유롭게

- 이 저작물을 복제, 배포, 전송, 전시, 공연 및 방송할 수 있습니다.

다음과 같은 조건을 따라야 합니다:



저작자표시. 귀하는 원저작자를 표시하여야 합니다.



비영리. 귀하는 이 저작물을 영리 목적으로 이용할 수 없습니다.



변경금지. 귀하는 이 저작물을 개작, 변형 또는 가공할 수 없습니다.

- 귀하는, 이 저작물의 재이용이나 배포의 경우, 이 저작물에 적용된 이용허락조건을 명확하게 나타내어야 합니다.
- 저작권자로부터 별도의 허가를 받으면 이러한 조건들은 적용되지 않습니다.

저작권법에 따른 이용자의 권리는 위의 내용에 의하여 영향을 받지 않습니다.

이것은 [이용허락규약\(Legal Code\)](#)을 이해하기 쉽게 요약한 것입니다.

[Disclaimer](#)

**Monitoring of Multi-phase Flow using Electrical Impedance
Tomography with Level Set-based Method**

Dong Liu

(Supervised by Professor Kyung Youn Kim)

A thesis submitted in partial fulfillment of the requirement for the
degree of Master of Science

2011. 06

The thesis has been examined and approved.

Thesis director, Sin Kim, Professor, Department of Nuclear and Energy Engineering

Min Jae Kang, Professor, Department of Electronic Engineering

Kyung Youn Kim, Professor, Department of Electronic Engineering

Date

**MAJOR OF ELECTRONIC ENGINEERING
FACULTY OF APPLIED ENERGY SYSTEM
GRADUATE SCHOOL
JEJU NATIONAL UNIVERSITY
REPUBLIC OF KOREA**

Contents

1. Introduction.....	1
1.1 Electrical impedance tomography.....	1
1.2 Shape reconstruction problem.....	3
1.3 Aims and contents of the thesis.....	6
2. Forward problem.....	7
2.1 Physical model inside the body.....	7
2.2 Complete electrode model.....	9
2.3 Numerical solution of forward problem.....	10
2.4 Jacobian calculation for resistivity change.....	14
3. Shape reconstruction in EIT.....	17
3.1 Level set method.....	18
3.1.1 Level set formulation for two-phase flow.....	18
3.1.2 General multi-phase formulation.....	19
3.1.3 Inverse problem using level set method.....	21
3.2 Jacobian calculation with level set function.....	22
3.3 Results and discussion.....	24
3.3.1 Numerical results.....	24
3.3.2 Experimental results.....	36
4. Conclusions.....	40
Summary.....	41
References.....	42

초록

전기 임피던스 단층촬영법(EIT)에서는 경계면의 전기적 측정치로부터 대상체 내부의 도전율 또는 유전율에 대한 영상이 얻어진다. 일반적으로, 대상체 주위에 일정한 간격으로 전도성 전극을 부착하고 이 전극들을 통해 소량의 전류를 주입시킨다. 이에 유기되는 전기 신호인 전압을 측정하는데, 이 과정을 여러 다른 전류 패턴들에 대해서 반복 수행한다. 그리고 주입시킨 전류와 측정 전압 데이터를 사용하여, 대상체 내부의 도전율 분포 또는 저항률 분포에 대한 근사치를 얻을 수 있다. 수학적으로, EIT 문제는 비선형이고 부정치성 역문제이다.

본 논문에서는, EIT 에서 level set 방법을 기반으로 한 다상류(multi-phase flow)에 대한 모양 복원(shape reconstruction) 방법을 제안한다. 이 방법의 주요 특징은 서로 다른 도전율 값을 갖는 영역들 사이의 경계를 찾는 역문제를 풀기 위해 협대역(narrowband) level set 방법을 사용하는 것이다. 다상 level set 모델을 사용함에 있어서, 도전율은 두 level set 함수에 의해 주어질 수 있다. 주요 아이디어는 level set 이론을 기반으로, 고차원 함수의 (zero) level set 으로서 모양의 경계(shape interface)를 나타내고 나서 편미분 방정식들의 집합을 푸는 것이다. level set 기반의 기법은 전형적인 픽셀 기반의 접근 방법과 비교해서 몇몇 이점들을 제공한다. level set 전략은 전개 과정 동안 저절로 위상기하학적 병합(topological merging)과 분리(breaking)를 다룬다. 다상의 경우에 대해 적용시키기 위해 level set 방법을 확장하였고, 수치적 데이터와 실험 데이터를 사용하여 제안 알고리즘을 테스트 하였다. 그 결과, 모양 기반의 level set 방법이 픽셀 기반의 영상 방법과 비교해서 더 나은 복원 성능을 보였다.

1. Introduction

1.1 Electrical impedance tomography

Electrical impedance tomography (EIT) is an imaging technique to view cross-sectional image of the object, where an array of electrodes are attached and small alternating current are injected and the corresponding voltages are measured, the internal conductivity or resistivity distribution is reconstructed with these measurement data from the boundary of the object to be imaged. A schematic diagram of the EIT measurement system is shown in figure 1.1. As EIT technology come from the soft field imaging techniques which the electrical quantities are dispersed inside the object and are affected by the inside objects, thus EIT has lower spatial resolution in comparison to other modalities, such as, magnetic resonance imaging (MRI) and X-ray tomography. On the other hand, EIT has high-speed data acquisition system thus has high temporal characteristics. For example in industrial process tomography, where the targets often change very rapidly, EIT is a workable modality due to its good temporal resolution.

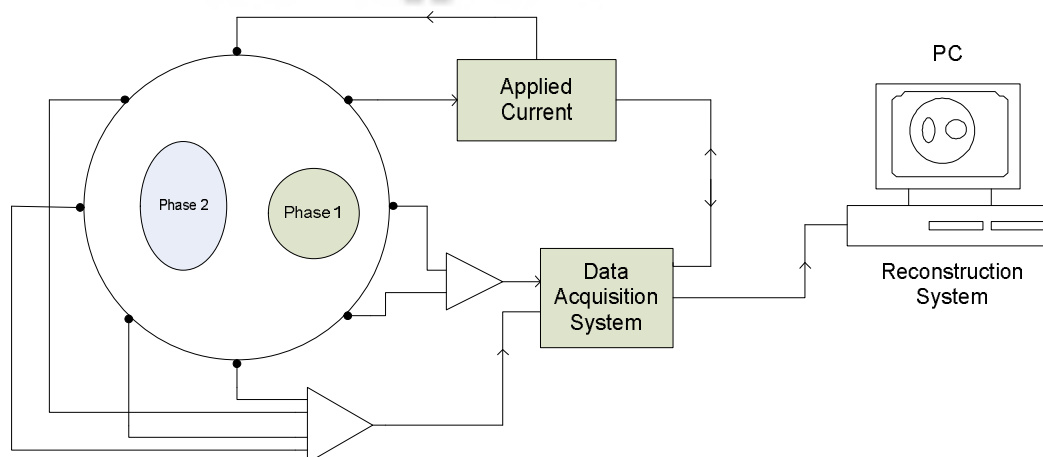


Figure 1.1 Schematic diagram of EIT system

Many applications of EIT have been developed e.g. for medical purpose. For instance, EIT is useful for monitoring patient lungs because the air has a large conductivity contrast to the other tissues in the thorax (Brown 2001). The most promising clinical application is for lung function monitoring of patients being treated with mechanical ventilation. EIT can resolve the changes in

the distribution of lung volumes between dependent and non-dependent lung regions as ventilator parameters are changed. Also EIT is being investigated in the field of breast imaging as an alternative or complementary technique to mammography and magnetic resonance imaging (MRI) for breast cancer detection (Cherepenin *et al.* 2001, Cherepenin *et al.* 2002 and Kerner *et al.* 2002). In industrial field, EIT has been widely applied to monitor flow processes, multi-phase imaging and monitor mixtures of conductive fluids in vessels or pipes (Jones *et al.* 1993).

In EIT, an image of the conductivity or resistivity distribution of the object is inferred from surface electrical measurements made on the boundary. Image reconstruction in EIT is a kind of nonlinear optimization problem, which means the solution is obtained iteratively and computed through forward and inverse solvers. In forward problem, the conductivity distribution and the injected current are known and the voltages are computed. In inverse problem, the internal conductivity distribution of the object is estimated based on the measured voltage and injected current data. The physical relationship between the internal conductivity or resistivity and measured boundary voltages is governed by a partial differential equation (PDE) derived from Maxwell equations with an appropriate boundary condition. Methods for reconstruction of EIT images are based on mathematical models that connect the internal conductivity or resistivity distribution to the voltages measurements made on the boundary of the object. In (Cheng *et al.* 1989) various models were studied, such as continuum, average-gap, shunt and complete electrode model (CEM). In connection with EIT problem these models are referred to as electrode models. It was found that the most accurate and popular model is CEM. This model can take into account the shunting effect of the electrodes and also the contact impedances between the electrodes and the object. In most cases, it is impossible to obtain an analytical solution for the forward problem so a numerical technique such as the finite element method (FEM) can be applied (Jain *et al.* 1997, Polydorides *et al.* 2002). The EIT reconstruction methods can be divided into two categories, *stationary* and *non-stationary imaging*. Stationary imaging techniques are used for the case where the internal conductivity of the object is time invariant within the time taken to acquire a full set of measurement data. In this thesis, reconstruction methods for the stationary cases are considered. In *non-stationary imaging* or *dynamic imaging technique*, which have been introduced to enhance the temporal resolution for situations where the conductivity distribution inside the body changes

rapidly. In these dynamic approaches, the time-dependence of the conductivity distribution is taken into account, and a reconstruction is obtained after each current injection. The reduction in current patterns is also made possible by the analysis of current patterns to use only the optimal current patterns in a dynamic scenario. With the evaluation of the norm and power distinguishability, the optimal current pattern can be determined (Isaacson 1990, Gisser *et al.* 1988). With or without using the optimal current patterns, many dynamic techniques were proposed in which the inverse problem is treated as a nonlinear state estimation problem and the time-varying state is estimated with a suitable reconstruction method, where the Kalman filter (KF) (Vauhkonen 1997, Kim *et al.* 2001) is the most popular method for tracking the dynamic changes.

1.2 Shape reconstruction problem

Two-phase or multi-phase flow can occur in a variety of industrial applications, such as in condensers, nuclear cooling systems, and fluidised bed sulphide roasters, heat exchangers, and oil pumping for example. The constituents may be gas and liquid, such as air/water or steam/water, gas and solid, as in a fluidised bed. Liquid/liquid immiscible flows occur in oil extraction, where oil mixes with water in the borehole. The phase distribution affects the safety, control and operation of mechanical systems and clinic treatment therefore it is necessary to determine the phase distribution without disturbing the flow field (figure 1.2).

In order to achieve even more voracious measurement information on two-phase flow section, and carry out non-intrusive and non-destructive collecting information, many novel sensor techniques have been applied to the measurement of two-phase flow, such as radiation (Banerjee *et al.* 1981), laser (Kumar *et al.* 1995), nuclear magnetic resonance (NMR) (Lynch *et al.* 1977), ultrasonic (Couthard *et al.* 1993), and tomography. One kind of attractive technique to measure two-phase flow parameters is a method based on electrical tomography. Such a method uses non-intrusive or non-invasive sensors that are located on the boundary of objects, such as process vessels or pipelines, to reconstruct the spatial distribution of the interfaces among various phases and then form the cross-sectional image of the phase distributions of objects. The electrical tomographic methods applied in two-phase flow measurement such as electrical capacitance tomography (ECT),

electrical resistivity tomography (ERT), and EIT have become popular. For example, ERT system was used to measure the gas–liquid mixture in a stirred vessel (Wang *et al.* 1999). An ERT system applied to monitor the hydro cyclone operation (Bond *et al.* 1999). Also measurement parameters of two-phase flow using ERT system has been studied (Dong *et al.* 2003). A real-time EIT system was used to image the flow of saline through the human vascular system (Brown *et al.* 1992), EIT system was used to image a volunteer's forearm during resting cardiovascular activity (Halter *et al.* 2008). In case of multi-phase flow, similar as two-phase flow, EIT can be a promising technique to reconstruct the phase distribution. In many situations, the knowledge of the conductivities of the anomalies is known *a priori*. The prior information of the conductivities can be used in the inverse algorithm to estimate the size, shape and location of the anomalies. The process of the estimating the phase distribution from the measured voltages made on the boundary is named as shape reconstruction problem.

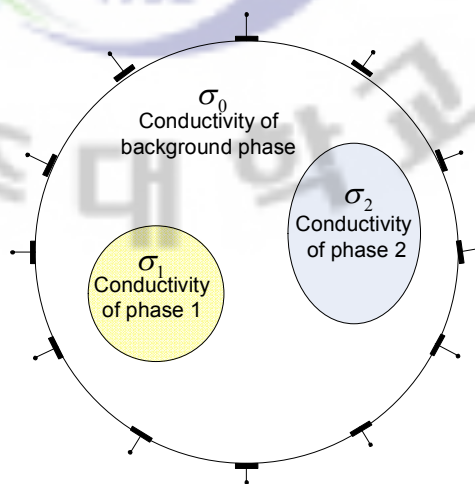


Figure 1.2 Shape reconstruction of multi-phase flow using EIT

Shape reconstruction has been studied by many researchers and different methods are proposed to represent the shape of the anomalies occurring in flow process (Tamburrino *et al.* 2003, Kolehmainen *et al.* 1999). Level set method has emerged recently as an attractive alternative to solve topology optimization problems (Osher *et al.* 1988). A level set representation can describe concisely the geometric and material boundaries of an anomaly, for example it can be used to represent or identify piecewise constant or piecewise smooth functions of the inclusions (Luminita *et al.* 2002, Osher *et al.* 2001 and Chung *et al.* 2005). More importantly, it has strong ability to accommodate shape related topological changes, especially merging or splitting of the

components. Level set method has become powerful and versatile tool for image processing and computational physics (Luminita *et al.* 2002, Osher *et al.* 2001 and Osher *et al.* 2003), also it has found applications in shape reconstruction and inverse scattering (Dorn *et al.* 2000, Dorn *et al.* 2006). More recently, applications of level set method to electrical tomography problems have been proposed. In Ito *et al.* 2001, using values of Neumann data as well as values of solution in a thin layer along the domain, level set method together with steepest descent method has been employed to solve the inverse conductivity problem. In Soleimani *et al.* 2006a, narrow band level set method applied in Gauss-Newton method as an inverse algorithm was used to estimate the shape and conductivities of two-phase. In Soleimani *et al.* 2006b, a similar method as in Soleimani *et al.* 2006a was employed using EIT to imaging of the human brain. Most of the work discussed before are related to the reconstruction of two-phase. In real situations, more than two-phase can exist, therefore, multi-phase reconstruction will provide better visualization of the flow characteristics.

In this thesis, we present shape reconstruction technique based on level set method using EIT. Multi-phase reconstruction is done where the conductivity values of the inhomogeneous background and that of anomalies are known, and the size, shape and location of the anomalies are unknown. Gauss Newton method based on level set method in Soleimani *et al.* 2006a and multi-phase framework for image segmentation in Luminita *et al.* 2002 are employed into multi-phase shape reconstruction. In using a multi-phase level set model, we will represent the conductivity by two level set functions. Based on the level set theory, the key idea was to implicitly represent the shape interface as the zero level set of a higher dimensional function, and then solve a set of partial differential equations in the Cartesian coordinate system which contains the shape of this new embedding function. The shape is set as the zero level set of higher dimensional functions, so the computational cost and time will increase. In order to reduce the cost time, we used a narrowband technique to calculate the shape deformation or update. The combination of the narrowband technique and optimization approach results in a computationally efficient and fast method for solving the inverse problem.

1.3 Aims and contents of the thesis

The aims of this thesis are:

1. To apply level set method for monitoring of multi-phase flow using EIT.
2. To investigate the performance of the proposed algorithm.
3. To evaluate the proposed approach with standard pixel-based Gauss Newton method using numerical and experimental data.

This thesis contains four chapters. Chapter 1 gives a soft introduction about EIT and shape reconstruction in general. The most commonly applied applications and methodology are given in this chapter and an overview of this thesis is given. In chapter 2 the most widely used EIT electrodes model, so-called complete electrode model (CEM), is presented and a finite element method (FEM) is applied to solve the forward problem of EIT. The solution of CEM, that is, the solution of the potential distribution when injected currents and conductivity or resistivity are known, is necessary in the implementation of inverse problem. Also the Jacobian calculation is discussed in this chapter. Chapter 3 constitutes the main part of this thesis, in which the novel shape-based level set method is applied to reconstruct the shape of the flow process. Several numerical simulations and experimental case for multi-phase flow are studied to demonstrate the performance of the proposed method. Finally, the conclusion and guidelines of the future research are summarized in chapter 4.

2. Forward problem

In order to solve an EIT reconstruction problem, a physical model need to be derived from the prior information, such as measured voltage, injected current, and a conductivity distribution. The equations for the physical model can be derived from Maxwell equations of electromagnetism (Malmivuo *et.al.* 1995, Doerstling 1995). In this chapter, the so-called complete electrode model (CEM) applied into governing equation with boundary conditions to solve the EIT problem is presented. The numerical solution for CEM is also given. Also Jacobian defined as the rate of change of potential with respect to the conductivity or resistivity is derived.

2.1 Physical model inside the body

Maxwell's equations in the domain Ω can be written as

$$\nabla \times E = -\frac{\partial B}{\partial t} \quad (2.1)$$

$$\nabla \times H = J + \frac{\partial D}{\partial t} \quad (2.2)$$

where E is the electric field, H magnetic field, D electric displacement, B magnetic induction, and J electric current density.

In case of linear isotropic medium domain Ω , the following equations holds true

$$D = \varepsilon E \quad (2.3)$$

$$B = \mu H \quad (2.4)$$

$$J = \sigma E \quad (2.5)$$

where ε is permittivity, μ permeability, and σ conductivity of the medium. Assuming that the injected currents are time harmonic with frequency ω and using the previous equations (2.3-2.5) we get the following relationships

$$E = \tilde{E}e^{i\omega t} \quad (2.6)$$

$$B = \tilde{B}e^{i\omega t} \quad (2.7)$$

Solving equations (2.1) and (2.2) using equations (2.3) to (2.7), we get

$$\begin{aligned} \nabla \times E &= -\frac{\partial B}{\partial t} = -\frac{\partial(\tilde{B}e^{i\omega t})}{\partial t} \\ &= -i\omega\tilde{B}e^{i\omega t} = -\frac{e^{i\omega t}\partial(\tilde{B})}{\partial t} = -i\omega\mu H - \frac{e^{i\omega t}\partial(\tilde{B})}{\partial t} \end{aligned}$$

$$\begin{aligned} \nabla \times H &= J + \frac{\partial D}{\partial t} = J + \frac{\partial(\epsilon E)}{\partial t} = J + \frac{\epsilon\partial(\tilde{E}e^{i\omega t})}{\partial t} \\ &= J + i\omega\epsilon\tilde{E}e^{i\omega t} + \frac{\epsilon e^{i\omega t}\partial(\tilde{E})}{\partial t} = J + i\omega\epsilon E + \frac{\epsilon e^{i\omega t}\partial(\tilde{E})}{\partial t} \end{aligned}$$

In EIT, the current density J can be divided into two components, which are so-called ohmic current ($J^0 = \sigma E$) and current source (J^s). The following simplified Maxwell equations can hold true without the oscillatory exponential terms (Somersalo *et al.* 1992, Ola *et al.* 1993, Doerstling 1995)

$$\nabla \times E = -i\omega\mu H \quad (2.8)$$

$$\nabla \times H = (\sigma + i\omega\epsilon)E + J^s. \quad (2.9)$$

In EIT, some simplifications are made for those equations, such as assuming static conditions, which mean that the effect of magnetic induction which produces an induced electric field is neglected. Also the capacitive effects $i\omega\epsilon E$ in (2.9) is assumed be neglected (Barber *et al.* 1984, Baker 1989). With these assumptions, the above equations can be simplified as

$$E = -\nabla u \quad (2.10)$$

$$\nabla \times H = \sigma E + J^s. \quad (2.11)$$

Taking the divergence on both sides of (2.11) and substituting (2.10) into (2.11), the equation

$$\nabla \cdot (\nabla \sigma u) = 0 \tag{2.12}$$

can be obtained for EIT inside the domain, where $u = u(x,y)$, for $x,y \in \Omega$. The equation (2.12) serves as the governing equation for EIT. In order to solve the governing equations, a set of boundary conditions need to be considered. In the following subsection, a so-called complete electrode model in EIT is presented.

2.2 Complete electrode model

In EIT problem, there are current source j_s on the boundary $\partial\Omega$ of the object Ω , we get the boundary condition:

$$\int_{e_\ell} \sigma \frac{\partial u}{\partial \nu} dS = I_\ell \quad \text{on } \partial\Omega_\ell, \quad \ell = 1, 2, \dots, L \tag{2.13}$$

In order to taking convenience on research of CEM, we set the zone between two electrodes by $\partial\Omega_h$, and assume that there is no current on $\partial\Omega_h$, so we get

$$\sigma \frac{\partial u}{\partial \nu} = 0 \quad \text{on } \partial\Omega_h \tag{2.14}$$

In actual application of EIT, we should take account of the imperfect contact between electrode and object, according series connection theorem (see figure 2.1), the real potential of electrode should be the plus of the potential at the object and the contact impedance potential. Described as:

$$u + z_\ell \sigma \frac{\partial u}{\partial \nu} = U_\ell \quad (x, y) \in e_\ell, \quad \ell = 1, 2, \dots, L \tag{2.15}$$

where z_ℓ is the effective contact impedance between the ℓ th electrode and object. U_ℓ is the measured boundary potential.

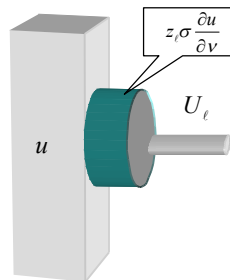


Figure 2.1 A zoom-in picture of one electrode and object

2.3 Numerical solution of forward problem

In section 2.2, equations set of CEM are obtained, the main goal is to find the potential $u(x, y)$ on Ω and the voltages U_ℓ on the electrodes with the information of the injected currents, measured boundary voltages and the prior knowledge on the resistivity values. With a small change of governing equation 2.12, and define $\Phi = \sigma \nabla u$, then

$$\nabla \cdot \Phi = \nabla \cdot (\sigma \nabla u) = 0 \quad (2.16)$$

Using a test function V to multiply equation (2.16), we can get

$$V \nabla \cdot \Phi = 0 \quad (2.17)$$

And integrating the equation (2.17) over the object Ω

$$\int_{\Omega} V \nabla \cdot \Phi dp = 0 \quad (2.18)$$

For $\int_{\partial\Omega} V \Phi ds = \int_{\Omega} \nabla \cdot (V \Phi) dp = \int_{\Omega} V \nabla \cdot \Phi dp + \int_{\Omega} \nabla V \cdot \Phi dp$ (if $\partial\Omega$ is smooth enough)

$$\text{Then} \quad \int_{\partial\Omega} V \sigma \nabla u ds = \int_{\Omega} \nabla V \cdot \sigma \nabla u dp \quad (2.19)$$

As we know, there is no current on $\partial\Omega_h$, thus equation (2.19) can be written that

$$\sum_{\ell=1}^L \int_{e_\ell} V \sigma \nabla u ds = \int_{\Omega} \nabla V \cdot \sigma \nabla u dp \quad (2.20)$$

Furthermore, the equation (2.15) implies

$$\sigma \nabla u = - \frac{u - U_\ell}{z_\ell} \quad (2.21)$$

Now the equation (2.20) can be written in the form

$$\sum_{\ell=1}^L \frac{1}{z_\ell} \int_{e_\ell} (u - U_\ell) V ds + \int_{\Omega} \sigma \nabla u \cdot \nabla V dp = 0 \quad (2.22)$$

Then

$$\int_{\Omega} \sigma \nabla u \cdot \nabla V dp + \sum_{\ell=1}^L \frac{1}{z_{\ell}} \int_{e\ell} u V ds - \sum_{\ell=1}^L \frac{U_{\ell}}{z_{\ell}} \int_{e\ell} V ds = 0 \quad (2.23)$$

Next, using equation (2.21) into boundary equation (2.13), we can get

$$\frac{1}{z_{\ell}} \int_{e\ell} (U_{\ell} - u) ds = I_{\ell} \quad (2.24)$$

For U_{ℓ} is a constant parameter, then

$$\frac{-1}{z_{\ell}} \int_{e\ell} u ds + \frac{U_{\ell}}{z_{\ell}} \int_{e\ell} ds = I_{\ell} \quad \text{Set } |e\ell| = \int_{e\ell} ds, \text{ where } |e\ell| \text{ is the area of the electrode } \ell.$$

Equation (2.24) becomes

$$\frac{-1}{z_{\ell}} \int_{e\ell} u ds + \frac{|e\ell|}{z_{\ell}} U_{\ell} = I_{\ell} \quad (2.25)$$

In general, most of the forward problem cannot be solved analytically, thus numerical methods have to be employed. In this thesis, we use the finite element method (FEM) to obtain the numerical solution for the forward problem. In the context of FEM, the domain Ω is discretized into small triangular elements and the finite dimensional approximations are written for the unknown functions. The potential distribution within the object Ω is approximated by the finite sum in the form of

$$u \approx u^h = \sum_{n=1}^N \Phi_n u_n \quad (2.26)$$

Also set $V = \Phi_m$, then equation (2.23) becomes

$$\int_{\Omega} \sigma \nabla \left(\sum_{n=1}^N \Phi_n u_n \right) \cdot \nabla \Phi_m dp + \sum_{\ell=1}^L \frac{1}{z_{\ell}} \int_{e\ell} \sum_{n=1}^N \Phi_n u_n \Phi_m ds - \sum_{\ell=1}^L \frac{U_{\ell}}{z_{\ell}} \int_{e\ell} \Phi_m ds = 0 \quad (2.27)$$

$$\sum_{n=1}^N u_n \left[\int_{\Omega} \sigma \nabla \Phi_n \cdot \nabla \Phi_m dp + \sum_{\ell=1}^L \frac{1}{z_{\ell}} \int_{e\ell} \Phi_n \Phi_m ds \right] - \sum_{\ell=1}^L \frac{U_{\ell}}{z_{\ell}} \int_{e\ell} \Phi_m ds = 0 \quad (2.28)$$

In matrix form, we can write as

$$\sum_{n=1}^N B_{n,m} u_n + \sum_{\ell=1}^L C_{\ell,m} U_{\ell} = 0 \quad (2.29)$$

Where

$$B_{n,m} = \int_{\Omega} \sigma \nabla \Phi_n \cdot \nabla \Phi_m dp + \sum_{\ell=1}^L \frac{1}{z_{\ell \ell}} \int \Phi_n \Phi_m ds$$

$$C_{\ell,m} = -\frac{1}{z_{\ell \ell}} \int \Phi_m ds$$

For equation (2.25), use $u \approx u^h = \sum_{n=1}^N \Phi_n u_n$, it becomes

$$\frac{-1}{z_{\ell \ell}} \int \sum_{n=1}^N \Phi_n u_n ds + \frac{|e\ell|}{z_{\ell \ell}} U_{\ell} = I_{\ell}$$

$$\sum_{n=1}^N u_n \frac{-1}{z_{\ell \ell}} \int \Phi_n ds + \frac{|e\ell|}{z_{\ell \ell}} U_{\ell} = I_{\ell}$$

Define $\bar{C}_{n,\ell} = \frac{-1}{z_{\ell \ell}} \int \Phi_n ds$, $D_{\ell} = \frac{|e\ell|}{z_{\ell \ell}}$, then

$$\sum_{n=1}^N \bar{C}_{n,\ell} u_n + D_{\ell} U_{\ell} = I_{\ell} \tag{2.30}$$

Finally, the following system of linear equations is obtained from the finite element formulation

$$\bar{A}\bar{X} = \bar{b} \tag{2.31}$$

Where

$$A = \begin{pmatrix} B & C \\ C^T & D \end{pmatrix}, \quad X = \begin{pmatrix} u \\ U \end{pmatrix}, \quad b = \begin{pmatrix} 0 \\ I \end{pmatrix}$$

That is

$$\begin{pmatrix} B & C \\ C^T & D \end{pmatrix} \begin{pmatrix} u \\ U \end{pmatrix} = \begin{pmatrix} 0 \\ I \end{pmatrix} \tag{2.32}$$

In EIT, the potentials at the electrodes can be expressed in a matrix form as

$$U^h = \begin{pmatrix} 1 & 1 & \dots & 1 \\ -1 & 0 & \dots & 0 \\ 0 & -1 & \dots & 0 \\ \vdots & \vdots & \ddots & \vdots \\ 0 & 0 & \dots & -1 \end{pmatrix} \begin{pmatrix} \bar{U}_1 \\ \bar{U}_2 \\ \vdots \\ \bar{U}_L \end{pmatrix} = N\bar{U}$$

Where $N = (n_1, n_2, \dots, n_{L-1}) = \begin{pmatrix} 1 & 1 & \dots & 1 \\ -1 & 0 & \dots & 0 \\ 0 & -1 & \dots & 0 \\ \vdots & \vdots & \ddots & \vdots \\ 0 & 0 & \dots & -1 \end{pmatrix}$, $\bar{U} = (\bar{U}_1 \ \bar{U}_2 \ \dots \ \bar{U}_L)^T$

Now, equation (2.32) can be written as

$$\begin{pmatrix} B & C \\ C^T & D \end{pmatrix} \begin{pmatrix} u \\ N\bar{U} \end{pmatrix} = \begin{pmatrix} 0 \\ I \end{pmatrix}$$

Using matrix transform, we can get

$$\begin{pmatrix} B & CN \\ N^T C^T & N^T DN \end{pmatrix} \begin{pmatrix} u \\ \bar{U} \end{pmatrix} = \begin{pmatrix} 0 \\ N^T I \end{pmatrix}$$

Set

$$\tilde{I} = N^T I = \begin{pmatrix} 1 & 1 & \dots & 1 \\ -1 & 0 & \dots & 0 \\ 0 & -1 & \dots & 0 \\ \vdots & \vdots & \ddots & \vdots \\ 0 & 0 & \dots & -1 \end{pmatrix}^T \begin{pmatrix} I_1 \\ I_2 \\ \vdots \\ I_L \end{pmatrix} = (I_1 - I_2, I_1 - I_3, \dots, I_1 - I_L)^T$$

Then

$$\begin{pmatrix} B & CN \\ N^T C^T & N^T DN \end{pmatrix} \begin{pmatrix} u \\ \bar{U} \end{pmatrix} = \begin{pmatrix} 0 \\ \tilde{I} \end{pmatrix} \tag{2.33}$$

Solving the equation (2.31) or equation (2.33) as $X = A^{-1}b$, the approximation solution for the forward problem is obtained.

The elements of the other matrices in matrix A are

$$B(i, j) = \int_{\Omega} \frac{1}{\rho} \nabla \varphi_i \cdot \nabla \varphi_j d\Omega + \sum_{\ell=1}^L \frac{1}{z_{\ell} e_{\ell}} \int \varphi_i \varphi_j dS, \quad i, j = 1, 2, \dots, N \tag{2.34}$$

$$C(i, j) = -\frac{1}{z_j e_j} \int \varphi_i dS, \quad i = 1, 2, \dots, N, \quad j = 1, 2, \dots, L \tag{2.35}$$

$$D(i, j) = \frac{\delta_{ij}}{z_i e_j} \int dS = \frac{\delta_{ij} |e_j|}{z_i} = \begin{cases} 0 & i \neq j \\ \frac{|e_j|}{z_j} & i = j \end{cases} \quad i, j = 1, 2, \dots, L \tag{2.36}$$

2.4 Jacobian calculation for resistivity change

Jacobian is defined as the rate of change of potential with respect to the conductivity or resistivity, the resulting matrix is defined as Jacobian matrix. In the applications of EIT, a set of current patterns should be used. Even with the consideration of the current patterns, the expression of the above equation will not be altered if the resistivity and the contact impedance do not depend on the current pattern. If P is the number of the current patterns, $u \in \mathfrak{R}^{N \times P}$, $\bar{U} \in \mathfrak{R}^{(L-1) \times P}$, and $\tilde{I} \in \mathfrak{R}^{L \times P}$.

In some cases, the voltages are measured only at some selected electrodes, not every electrode. Also, the selected electrodes may be different at each current pattern. The measured voltages at the measurement electrodes U can be obtained as

$$U = M^T U^h = M^T N \bar{U} \in \mathfrak{R}^{E \times P} \quad (2.37)$$

where, E is the number of the measurement electrodes and $M \in \mathfrak{R}^{L \times E}$ is the measurement matrix. The element $M(\ell, p)$ is set to '1' if the ℓ -th electrode is measured at the p -th current pattern and otherwise set to zero. Furthermore, U^h can be extracted directly from X by introducing the extended mapping matrix \tilde{N}

$$\tilde{N} = (0, N) \in \mathfrak{R}^{L \times (N+L-1)} \quad \text{and} \quad U^h = \tilde{N} X \quad (2.38)$$

where $0 \in \mathfrak{R}^{L \times N}$. Therefore, we have

$$U = M^T U^h = M^T \tilde{N} X = \tilde{M} X \quad (2.39)$$

where the extended measurement matrix is defined as

$$\tilde{M} = M^T \tilde{N} \in \mathfrak{R}^{E \times (N+L-1)} \quad (2.40)$$

The Jacobian defined as the relative change of the measured voltage at the ℓ -th measurement electrode at the p -th current pattern (\hat{U}_ℓ^p) with respect to the change of the conductivity or resistivity of the m -th pixel (ρ_m), that is

$$J_{lpm} = \frac{\partial \hat{U}_l^p}{\partial \rho_m} \quad (2.41)$$

or in a matrix form

$$J = \begin{pmatrix} \frac{\partial \hat{U}_1^1}{\partial \rho_1} & \frac{\partial \hat{U}_1^1}{\partial \rho_2} & \dots & \frac{\partial \hat{U}_1^1}{\partial \rho_M} \\ \frac{\partial \hat{U}_2^1}{\partial \rho_1} & \frac{\partial \hat{U}_2^1}{\partial \rho_2} & \dots & \frac{\partial \hat{U}_2^1}{\partial \rho_M} \\ \vdots & \vdots & \vdots & \vdots \\ \frac{\partial \hat{U}_E^1}{\partial \rho_1} & \frac{\partial \hat{U}_E^1}{\partial \rho_2} & \dots & \frac{\partial \hat{U}_E^1}{\partial \rho_M} \\ \frac{\partial \hat{U}_1^2}{\partial \rho_1} & \frac{\partial \hat{U}_1^2}{\partial \rho_2} & \dots & \frac{\partial \hat{U}_1^2}{\partial \rho_M} \\ \vdots & \vdots & \vdots & \vdots \\ \frac{\partial \hat{U}_E^2}{\partial \rho_1} & \frac{\partial \hat{U}_E^2}{\partial \rho_2} & \dots & \frac{\partial \hat{U}_E^2}{\partial \rho_M} \\ \vdots & \vdots & \vdots & \vdots \\ \frac{\partial \hat{U}_E^p}{\partial \rho_1} & \frac{\partial \hat{U}_E^p}{\partial \rho_2} & \dots & \frac{\partial \hat{U}_E^p}{\partial \rho_M} \end{pmatrix} \quad (2.42)$$

where M is the number of pixels (meshes). The Jacobian matrix can be obtained from the derivative of the system of equation

$$AX = b \quad (2.43)$$

and the expression

$$U = M^T U^h = M^T \tilde{N} X = \tilde{M} X \quad (2.44)$$

That is,

$$\begin{aligned} \frac{\partial U}{\partial \rho_m} &= \tilde{M} \frac{\partial X}{\partial \rho_m} = \tilde{M} \frac{\partial}{\partial \rho_m} (A^{-1}b) = \tilde{M} \frac{\partial A^{-1}}{\partial \rho_m} b \\ \frac{\partial A^{-1}}{\partial \rho_m} b &= -A^{-1} \frac{\partial A}{\partial \rho_m} A^{-1}b = -A^{-1} \frac{\partial A}{\partial \rho_m} X \\ \frac{\partial U}{\partial \rho_m} &= -\tilde{M} A^{-1} \frac{\partial A}{\partial \rho_m} X = -\left((A^{-1})^T \tilde{M}^T \right)^T \frac{\partial A}{\partial \rho_m} X = -\left(A^{-1} \tilde{M}^T \right)^T \frac{\partial A}{\partial \rho_m} X \end{aligned} \quad (2.45)$$

In the last equality, $(A^{-1})^T = A^{-1}$ is used because of the symmetry of the stiffness matrix. If the

pseudo-resistance matrix defined as

$$\tilde{R} = A^{-1} \tilde{M}^T \in \mathfrak{R}^{(N+L-1) \times E} \quad (2.46)$$

is given we can calculate the Jacobian matrix. The pseudo-resistance matrix can be easily obtained during the solution of the system equation

$$A \begin{pmatrix} \tilde{R} & X \end{pmatrix} = \begin{pmatrix} \tilde{M}^T & b \end{pmatrix} \quad (2.47)$$

or

$$A \begin{pmatrix} \tilde{R}_1 & u \\ \tilde{R}_2 & \tilde{U} \end{pmatrix} = \begin{pmatrix} 0 & 0 \\ N^T M & N^T b \end{pmatrix} \quad (2.48)$$

where

$$\tilde{R}_1 = \tilde{R}(1:N, :) \in \mathfrak{R}^{N \times E} \quad \text{and} \quad \tilde{R}_2 = \tilde{R}(N+1:N+L-1, :) \in \mathfrak{R}^{(L-1) \times E} \quad (2.49)$$

The derivative of the stiffness matrix with respect to the resistivity is

$$\frac{\partial A}{\partial \rho_m} = \begin{pmatrix} \frac{\partial B}{\partial \rho_m} & 0 \\ 0 & 0 \end{pmatrix} \quad (2.50)$$

Therefore, we have

$$\frac{\partial U}{\partial \rho_m} = - \begin{pmatrix} \tilde{R}_1 \\ \tilde{R}_2 \end{pmatrix}^T \begin{pmatrix} \frac{\partial B}{\partial \rho_m} & 0 \\ 0 & 0 \end{pmatrix} \begin{pmatrix} u \\ \tilde{U} \end{pmatrix} = - \begin{pmatrix} \tilde{R}_1^T & \tilde{R}_2^T \end{pmatrix} \begin{pmatrix} \frac{\partial B}{\partial \rho_m} u \\ 0 \end{pmatrix} = - \tilde{R}_1^T \frac{\partial B}{\partial \rho_m} u \quad (2.51)$$

in which the term $\frac{\partial B(i, j)}{\partial \rho_m}$ can be calculated as

$$\frac{\partial B(i, j)}{\partial \rho_m} = - \frac{1}{\rho_m^2} \int_{\Omega_m} \nabla \varphi_i \cdot \nabla \varphi_j d\Omega, \quad i, j = 1, 2, \dots, N \quad (2.52)$$

where φ_i, φ_j are basis functions and Ω_m is the element with which the derivative is computed.

3. Shape reconstruction in EIT

In EIT, the conductivity or resistivity distribution of the object is inferred from surface voltage measurements made on the boundary and the injected current data. Image reconstruction in EIT is a kind of nonlinear optimization problem, which means the solution is obtained iteratively and computed through forward and inverse solvers. The physical relationship between the internal conductivity or resistivity and measured boundary voltages is governed by a partial differential equation derived from Maxwell Equations with an appropriate boundary condition. For solving the nonlinear system equations, lots of classical method are applied to the impedance reconstruction (Li *et al.* 2004, Wang *et al.* 2004), such as modified Newton-Raphson method (mNR), Landweber method (LW), and Differential Evolution algorithm (DE). Recently, various methods that have been proven successful in image processing have also found their way to help solving electrical tomography problems. In this chapter, shape reconstruction based on level set method using EIT is presented. Multi-phase reconstruction is done where the conductivity values of the inhomogeneous background and that of anomalies are known, and the size, shape and location of the anomalies are unknown. Gauss-Newton method based on level set method in Soleimani *et al.* 2006a and multi-phase framework for image segmentation in Luminita *et al.* 2002 are employed to monitor the process of multi-phase flow. In using a multi-phase level set model, the conductivities distribution can be presented by two level set functions. Based on the level set theory, the inverse boundary problem is to find a level set function which can implicitly represent the conductivity distribution, and then solve a set of partial differential equations in the Cartesian coordinate system which contains the shape of this new embedding function to minimize the mismatch between the measured and calculated data. As the shape is described by the zero level set of higher dimensional functions, so the computational cost and time will increase. To improve the level set reconstruction process, a narrowband technique applied to calculate the shape deformation or update. The combination of the narrowband technique and optimization approach results in a computationally efficient and fast method for solving the inverse problem.

3.1 Level set method

3.1.1 Level set formulation for two-phase flow

For simplicity, we formulate the simpler two-phase problem first for a clearer introduction of the level set method in two dimensions, and then extend the framework to multi-phase problems. The interface represented by a level set function is thus also referred to as a curve. However, the methodology presented in this section can be naturally extended to any number of space dimensions. There, the interface that is represented is generally called a hyper surface (in three dimensions, it is simply called a surface). We will use the words interface and curves, interchangeably. In the level set method, the curves are implicitly defined as the zeros of a Lipschitz continuous function ϕ . This is to say that $\partial D := \{(x, y) : \phi(x, y) = 0\}$ corresponds to the embedded curve. See Figures 3.1 for example.

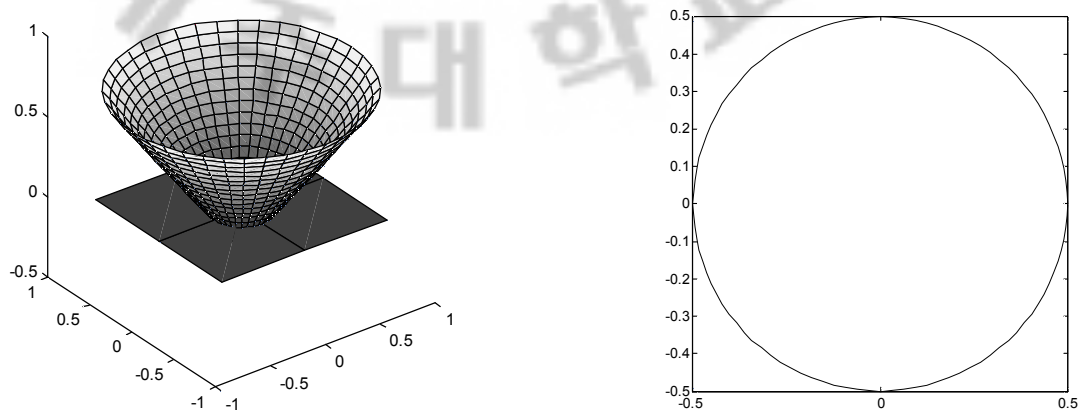


Figure 3.1 A circular contour embedded by a level set function.

If D is the inclusion with conductivity σ_{int} embedded in a background Ω with conductivity σ_{ext} , then the embedded curve, which is the boundary $\Gamma = \partial D$ of the inclusion, can be given by the zero level set

$$\partial D := \{(x, y) : \phi(x, y) = 0\} \quad (3.1)$$

where the conductivity distribution of each point will be

$$\sigma(x, y) = \begin{cases} \sigma_{\text{int}} & \{(x, y) : \phi(x, y) < 0\} \\ \sigma_{\text{ext}} & \{(x, y) : \phi(x, y) > 0\} \end{cases} \quad (3.2)$$

If we add some perturbation on the level set function, which will lead in the change of the shapes automatically. This relationship is used in the level set technique when constructing updates to a given level set function such that the shapes are deformed in a way which reduces a given cost functional. We assume a continuous velocity field $v(t)$ whose restriction onto the curve represents the velocity of the curve, and then at least locally in time, the evolution can be described as a Hamilton-Jacobi-type equation

$$\frac{\partial \phi}{\partial t} + v(t)|\nabla \phi| = 0 \quad (3.3)$$

Here $v(t)$ is a velocity function of evolving contours in their outward direction. we assume the velocity field is regular enough smooth that the basic structure of shape D remains preserved during this evolution. Meantime we assume that $|\nabla \phi|$ is well defined and nonzero along the shape boundary represented by a smooth level function $\phi(x, y)$. For solving equation (3.3), usually an approach of steepest descent flow can be applied. See for example (Burger 2001, Ito *et al.* 2001).

3.1.2 General multi-phase formulation

In this subsection, the shape parameterization using level set method is presented. With m level set functions $(\phi_1, \phi_2, \phi_3, \dots, \phi_K)$, we can represent up to 2^m distinct regions of the form $\bigcap_{j=1}^m \{\pm \phi_j > 0\}$ (Luminita *et al.* 2002), and each may be used to represent one phase. For simplicity of presentation, we assume Ω contains three different regions (Figure 3.2) which did not have overlapping and vacuum state with piecewise constant conductivities $\sigma = (\sigma_0, \sigma_1, \sigma_2)$, where σ_0 , σ_1 and σ_2 are three positive real numbers. In association with the three regions given by the two level set functions $\phi = (\phi_1(x, y), \phi_2(x, y))$ through the representation of the interior conductivity distribution $\sigma(x, y)$ in Ω as follows.

$$\sigma = \sigma_0 H(\phi_1)H(\phi_2) + \sigma_1(1-H(\phi_1))H(\phi_2) + \sigma_2(1-H(\phi_2))H(\phi_1) \quad (3.4)$$

where $H(x)$ is the Heaviside function, namely

$$H(x) = 1 \quad \text{for } x \geq 0, \quad H(x) = 0 \quad \text{for } x < 0. \quad (3.5)$$

and $\phi = (\phi_1(x, y), \phi_2(x, y))$ is the level set function satisfying

$$\begin{aligned} \Omega_1 &= \{(x, y) \in \Omega \mid \phi_1(x, y) < 0, \phi_2(x, y) > 0\} \\ \Omega_2 &= \{(x, y) \in \Omega \mid \phi_1(x, y) > 0, \phi_2(x, y) < 0\} \end{aligned} \quad (3.6)$$

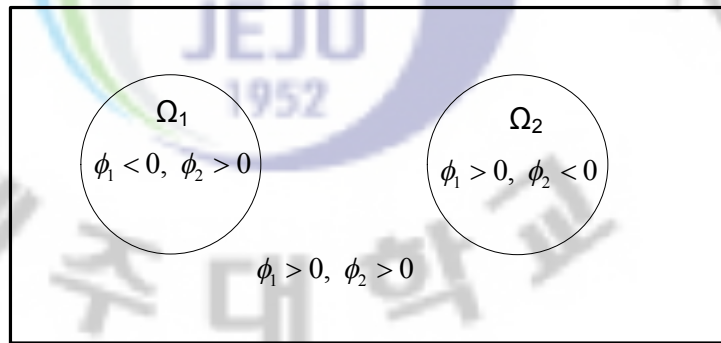


Figure 3.2 Example of partition of the domain in regions with boundaries represented via two level set functions

Then we can write

$$\nabla \sigma = g_1(\phi_2) \cdot \nabla H(\phi_1) + g_2(\phi_1) \cdot \nabla H(\phi_2) \quad (3.7)$$

Where

$$\begin{aligned} g_1(\phi_2) &= (\sigma_0 - \sigma_1)H(\phi_2) + \sigma_2(1-H(\phi_2)) \\ g_2(\phi_1) &= (\sigma_0 - \sigma_2)H(\phi_1) + \sigma_1(1-H(\phi_1)) \end{aligned} \quad (3.8)$$

Let Γ_j ($j = 1, 2$) be the interface between two different regions, which is also a boundary of the region, is given by the zero level set (Figure 3.3)

$$\partial\Gamma_j := \{(x, y) : \phi_j(x, y) = 0\} \tag{3.9}$$

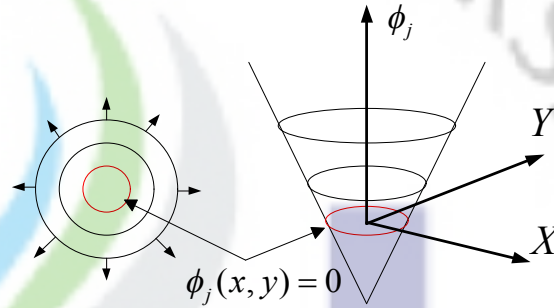


Figure 3.3 Representation of the expanding contours of the object as the zero level set of a level set function.

3.1.3 Inverse problem using level set method

If we change the level set function by a small distance, we assume the update is sufficiently smooth, such that the basic structure of the shape remains preserved. Then we move the shapes accordingly. This idea is used in the level set technique when constructing updates to a given level set function such that the shapes are deformed in a way which reduces the objective function. As given in Soleimani *et al.* 2006a, the Gauss-Newton update for level set function can be written as follows

$$\phi_{n+1} = \phi_n + \lambda(J_n^T J_n + \alpha^2 R^T R)^{-1} [J_n^T (V - G(\phi_n)) - \alpha^2 R^T R(\phi_n - \phi^*)] \tag{3.10}$$

Here J_n is the Jacobian calculated with ϕ_n being the level set function (detail of the Jacobian calculation will be discussed in the next section), V and $G(\phi_n)$ are the vector of measured and calculated voltages. λ is the time step size for the current update and R is a regularization matrix. To improve the level set reconstruction process, a narrowband technique applied to calculate the shape deformation or update. Here the narrow band means the area that includes elements sharing nodes with the boundary and its neighbors. It was able to reduce the number of elements taking part in the reconstruction process making it better conditioned. The level set-based reconstruction algorithm steps applied to multi-phase case are as follows:

1. Start with two initial guesses for the shape of the inclusions, namely two initial level set functions. During the following numerical or experimental solutions, distance functions are selected as level set functions.
2. Define the boundary of inclusions and narrow band. Solve 2D forward problem using FEM and calculate the updated Jacobian with respect to the level set function.
3. Update the level set function with an applicable step-size (such as using a line search technique) and calculate the new boundary of the inclusion and narrow band using the updated level set function.
4. Check the misfit condition of the logical. If it is satisfy enough, stop.
5. In case the misfit is not satisfied with the condition, go to step 2 until the final results are estimated.

All these steps are summarized in the following flowchart, see details in figure 3.4.

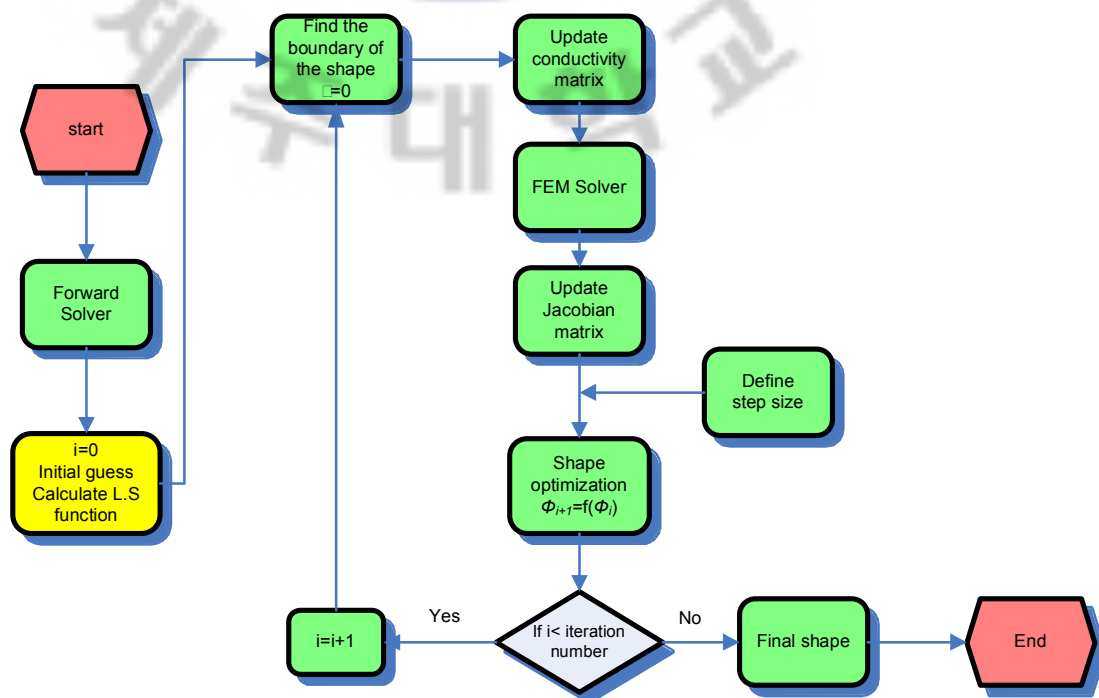


Figure 3.4 Flowchart of level set-based reconstruction algorithm.

3.2 Jacobian calculation with level set function

The Jacobian quantifies the sensitivity of the voltage measurements due to changes of the level set function, as an adaptive parameter in particular, the element conductivity changes. In this section,

a formula for the voltage sensitivity $\frac{\partial U}{\partial \phi_n}$ is derived, and we describe how this quantity is

assembled into each component of the Jacobian.

A change in the level set function of an element k requires the calculation of

$$J_k = \frac{\partial U}{\partial \phi_k} = \frac{\partial U}{\partial \sigma} \cdot \frac{\partial \sigma}{\partial \phi_k} \quad (3.11)$$

where

$$\sigma = \sigma_0 H(\phi_1) H(\phi_2) + \sigma_1 (1 - H(\phi_1)) H(\phi_2) + \sigma_2 (1 - H(\phi_2)) H(\phi_1)$$

Then the following relationships will be hold true

$$\begin{aligned} J_1 &= \frac{\partial U}{\partial \sigma} \cdot \frac{\partial \sigma}{\partial \phi_1} \\ &= \frac{\partial U}{\partial \sigma} \cdot [\sigma_0 (\delta(\phi_1) \cdot H(\phi_2)) - \sigma_1 \delta(\phi_1)] \\ &= \frac{\partial U}{\partial \sigma} \cdot (\sigma_0 - \sigma_1) \delta(\phi_1) \end{aligned} \quad (3.12)$$

and

$$\begin{aligned} J_2 &= \frac{\partial U}{\partial \sigma} \cdot \frac{\partial \sigma}{\partial \phi_2} \\ &= \frac{\partial U}{\partial \sigma} \cdot [\sigma_0 (\delta(\phi_2) \cdot H(\phi_1)) - \sigma_2 \delta(\phi_2)] \\ &= \frac{\partial U}{\partial \sigma} \cdot (\sigma_0 - \sigma_2) \delta(\phi_2) \end{aligned} \quad (3.13)$$

In the above, $\delta(x)$ denotes the Dirac function. Also from the previous chapter we can get

$$\frac{\partial U}{\partial \sigma} = - \begin{pmatrix} \tilde{R}_1 \\ \tilde{R}_2 \end{pmatrix}^T \begin{pmatrix} \frac{\partial B}{\partial \sigma} & 0 \\ 0 & 0 \end{pmatrix} \begin{pmatrix} u \\ \tilde{U} \end{pmatrix} = - \begin{pmatrix} \tilde{R}_1^T & \tilde{R}_2^T \end{pmatrix} \begin{pmatrix} \frac{\partial B}{\partial \sigma} u \\ 0 \end{pmatrix} = - \tilde{R}_1^T \frac{\partial B}{\partial \sigma} u \quad (3.14)$$

and

$$\frac{\partial B}{\partial \sigma} = \int_{\Omega_m} \nabla \varphi_i \cdot \nabla \varphi_j d\Omega \quad (3.15)$$

3.3 Results and discussion

In this section, imaging of multi-phase flow using level set method is presented. The method is tested with numerical and experimental data. In order to evaluate the performance of the proposed method, root mean square error (RMSE) as a performance criterion is computed. RMSE for conductivity distribution and voltage measurement are defined as

$$RMSE_{\sigma} = \frac{\|\sigma_{cal} - \sigma_{tru}\|}{\sigma_{tru}} \quad (3.16)$$

$$RMSE_u = \frac{\|u_{cal} - u_{tru}\|}{u_{tru}} \quad (3.17)$$

3.3.1 Numerical results

In this section, the numerical results obtained using level set methods are proposed. We carried out extensive computer simulations with synthetic data to illustrate the reconstruction performance of the proposed algorithm. In order to avoid the so-called ‘*inverse crime*’, two different finite element meshes are used for forward and inverse problem. A fine mesh (radius of 14 cm) with 3809 nodes and 7306 triangular elements is used in forward solver to generate the boundary voltage data. A coarse mesh with 985 nodes and 1840 triangular elements are used in inverse solvers to reconstruct the shape, location and size of the targets, see figure 3.5.

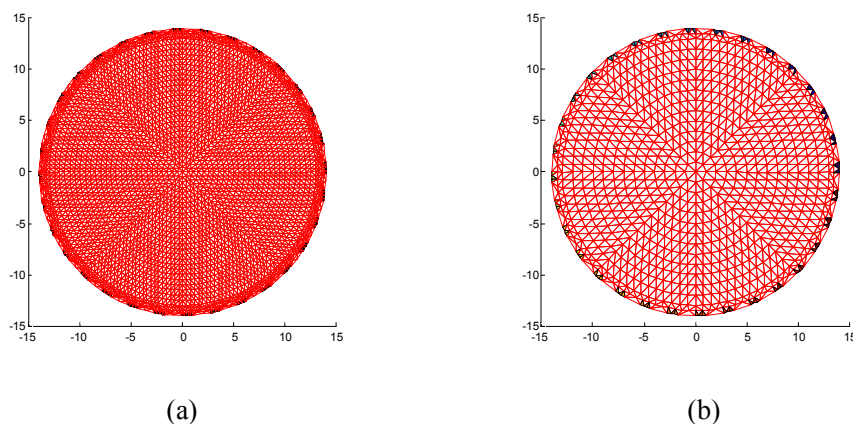


Figure 3.5 The used FEM mesh: (a) forward mesh and (b) inverse mesh.

In the first numerical example below, in figure 3.6 the background conductivity is set to 50mS/cm and the conductivity of the inclusions are set to 25mS/cm and 20mS/cm, respectively. With two different circles initial guess, solid line represents the true boundary, while the dashed line shows the initial guess, see figure 3.6(b), the level set method was able to identify the position and a relatively accurate shape of the inclusions. To simulate with actual conditions, Gaussian noise with S.D up to 2% of the corresponding computed voltage are added to the computed data. Reconstructed images of resistivity distribution without or with noise cases are shown in figure 3.6. Two criteria of the performance during the reconstruction are shown in figure 3.7 and figure 3.8, respectively.

In the next two examples (figure 3.9 and figure 3.12), we attempt to reconstruct two objects which are produced probability in industrial process tomography. Considering the actual conditions, Gaussian noise with S.D of 0.5%, 1% and 2% of the corresponding calculated voltage are added to the simulated data. The level set method was able to separate the inclusions clearly, and also identify the position and a good amount of details of the inclusions, see details in figure 3.9 and figure 3.12. The RMSE values of conductivity distribution during the shape reconstruction process are shown in figure 3.10 and figure 3.13, respectively. The RMSE plots of the voltage measurements of case 2 is shown in figure 3.11. The evolution of the shape during the level set reconstruction of case 4, in which inclusions are located relatively close to each other, are shown in figure 3.14. It is interesting to find that the two inclusions could be clearly imaged in the level set-based reconstruction. In case of using a standard regularized pixel-based method, it is difficult to separate those two inclusions. The RMSE value of conductivity distribution and voltage during the shape reconstruction process are shown in figure 3.15. In order to evaluate the performance of level set method, a comparison between level set method and modified Newton-Raphson method is studied in figure 3.16, in which different examples using simulation data are considered. It was found that level set method can easily separate two or more objects which are close to each other and mNR has a poor reconstruction in these cases. The results of level set-based reconstruction using narrow band technique largely depend on the choice of the regularization parameter α and initial guess, here the regularization parameter α not only take charge of the regularization function but also the smooth function. With a choice of $\alpha = 0.05$, we were able to recover the true

shape at noise level up to 2% with a quite accurate result. The optimal choice of initial guess is a very interesting problem as the level set function has a different significance for the reconstruction than the parameter distribution itself, for simplicity, distance functions are selected as level set functions in our numerical and experimental study.

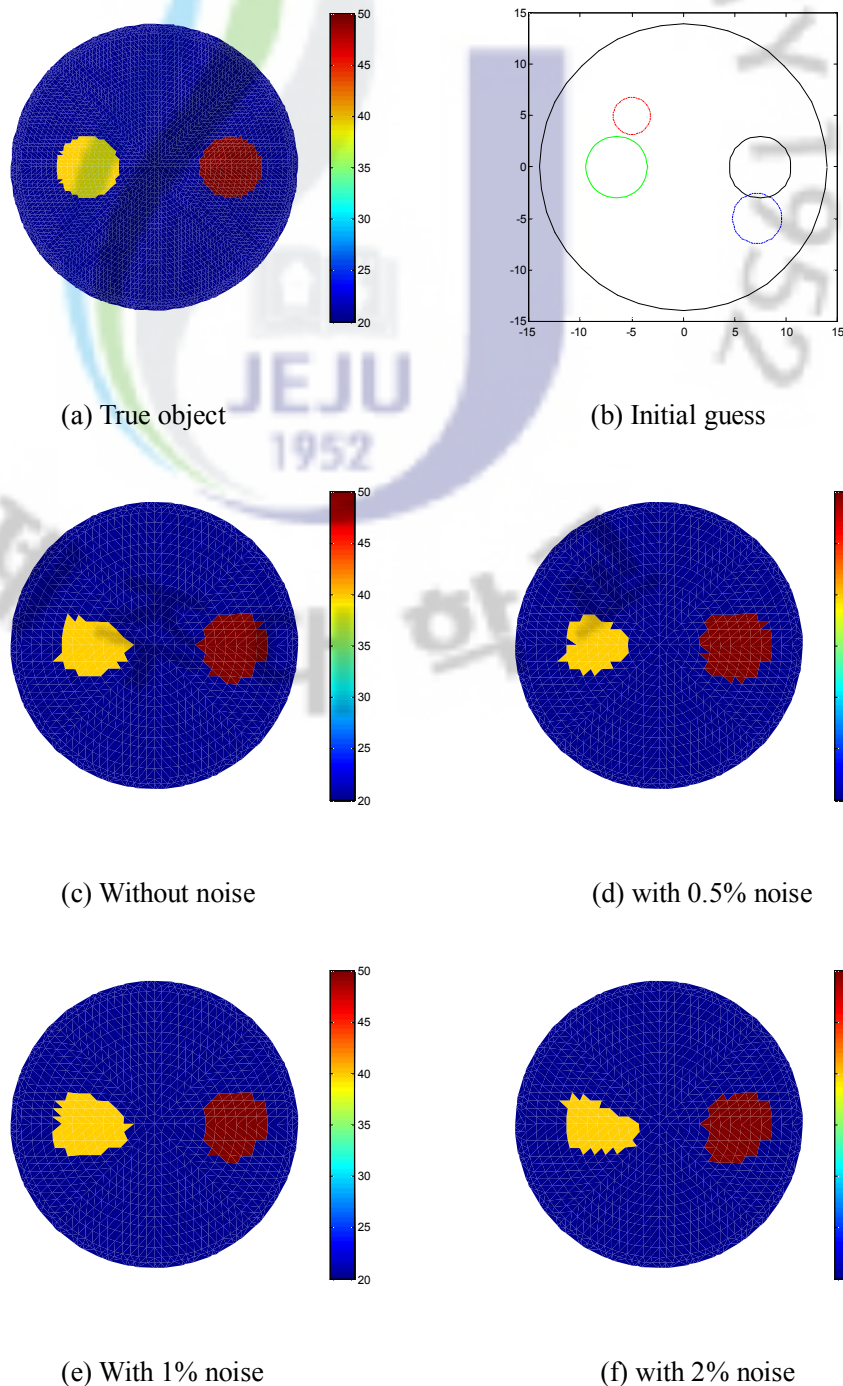
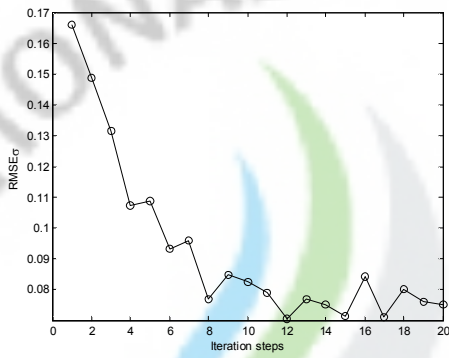
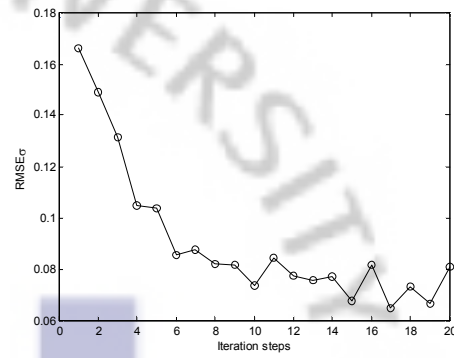


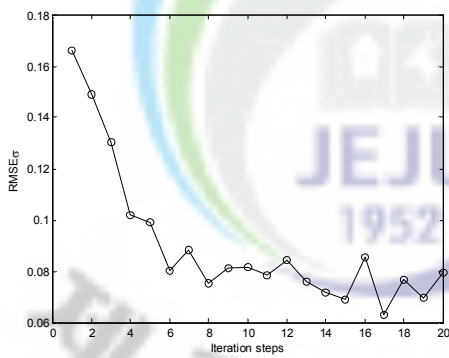
Figure 3.6 True image of resistivity distribution, initial guess (solid line represents the true boundary, while the dashed line shows the initial guess) and final level set reconstruction for case 1 with or without noise.



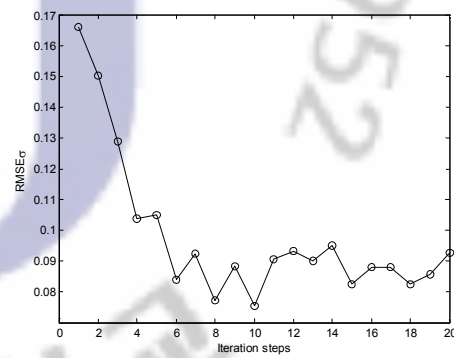
(a) Without noise



(b) with 0.5% noise

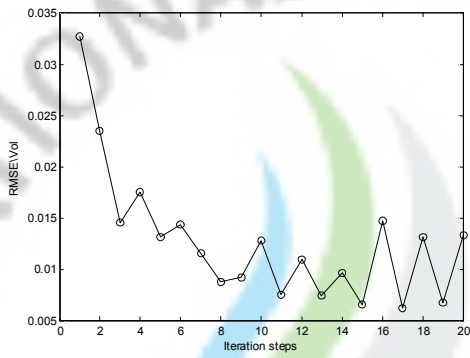


(c) With 1% noise

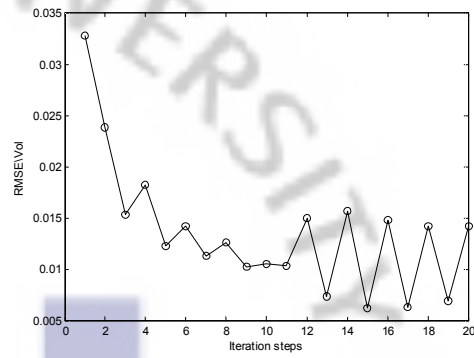


(d) with 2% noise

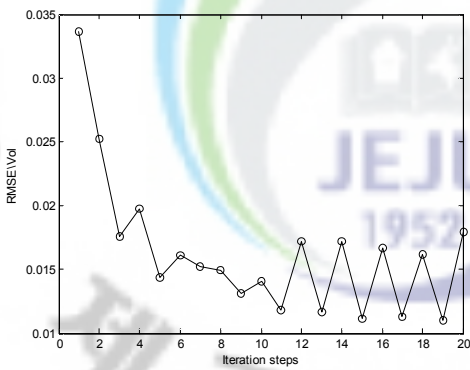
Figure 3.7 RMSE value of conductivity distribution of case 1 on different noise condition.



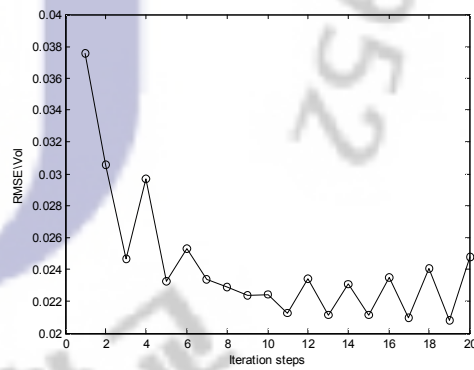
(a) Without noise



(b) with 0.5% noise



(c) With 1% noise



(d) with 2% noise

Figure 3.8 RMSE value of voltage of case 1 on different noise condition.

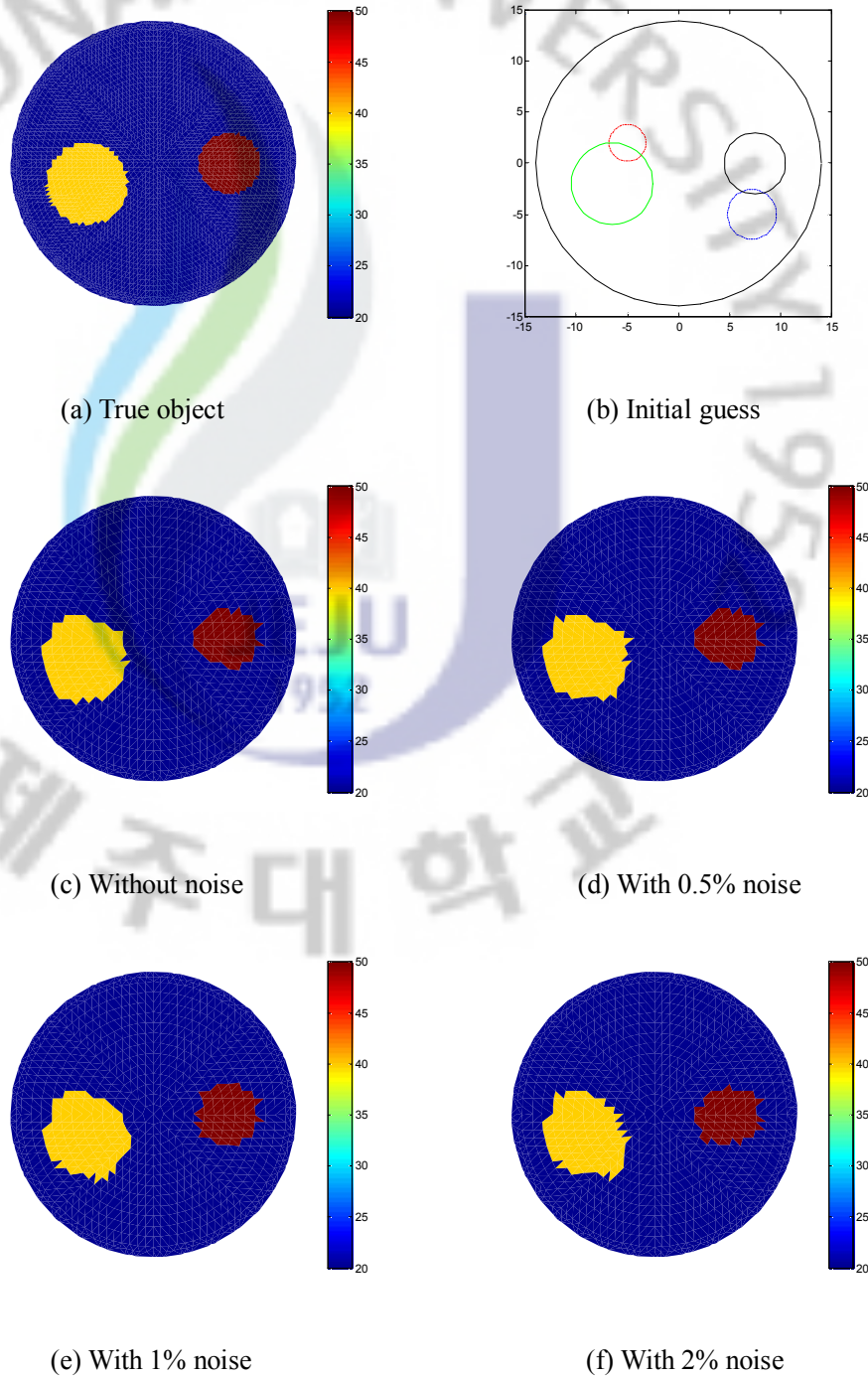
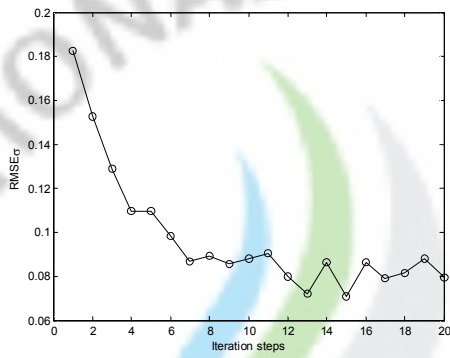
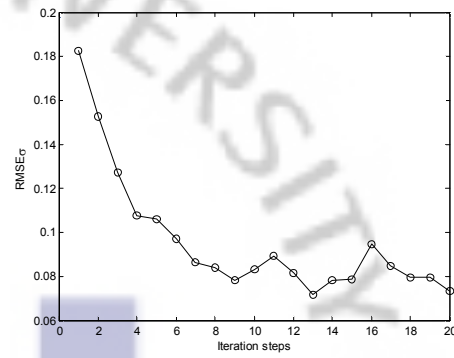


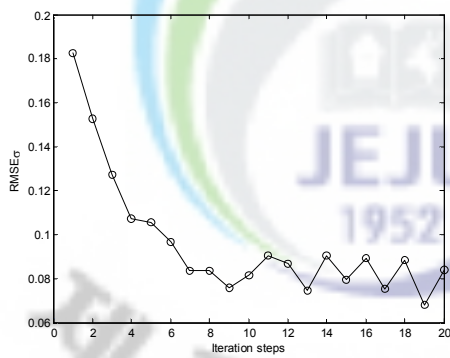
Figure 3.9 True image of resistivity distribution, initial guess (solid line represents the true boundary, while the dashed line shows the initial guess) and final level set reconstruction for case 2 with or without noise.



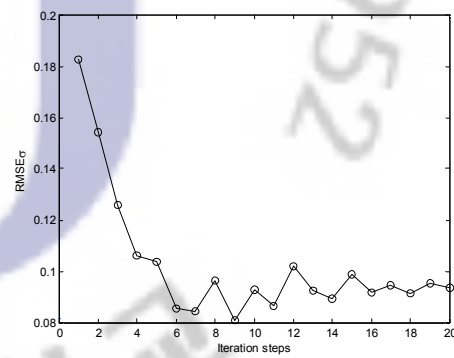
(a) Without noise



(b) With 0.5% noise

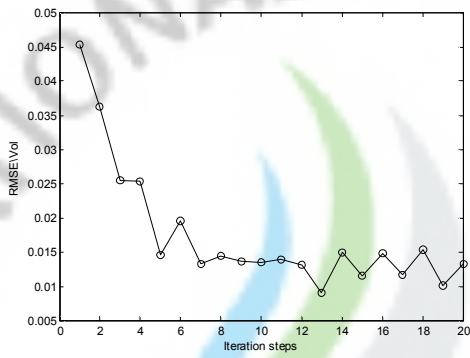


(c) With 1% noise

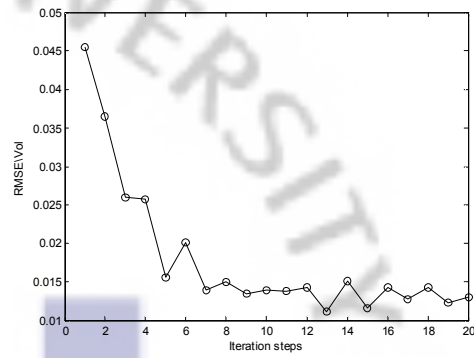


(d) With 2% noise

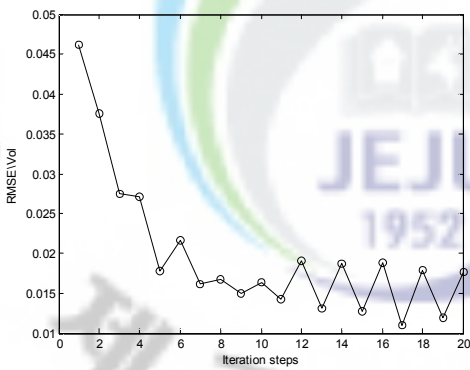
Figure 3.10 RMSE value of conductivity distribution of case 2 on different noise condition.



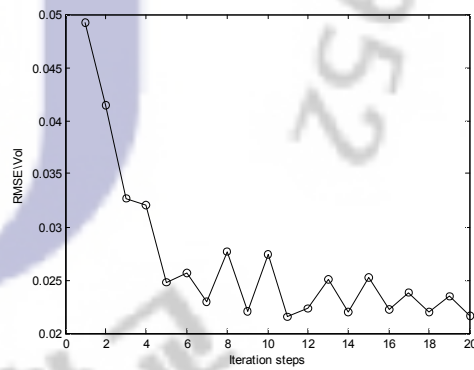
(a) Without noise



(b) With 0.5% noise



(c) With 1% noise



(d) With 2% noise

Figure 3.11 RMSE value of voltage of case 2 on different noise condition.

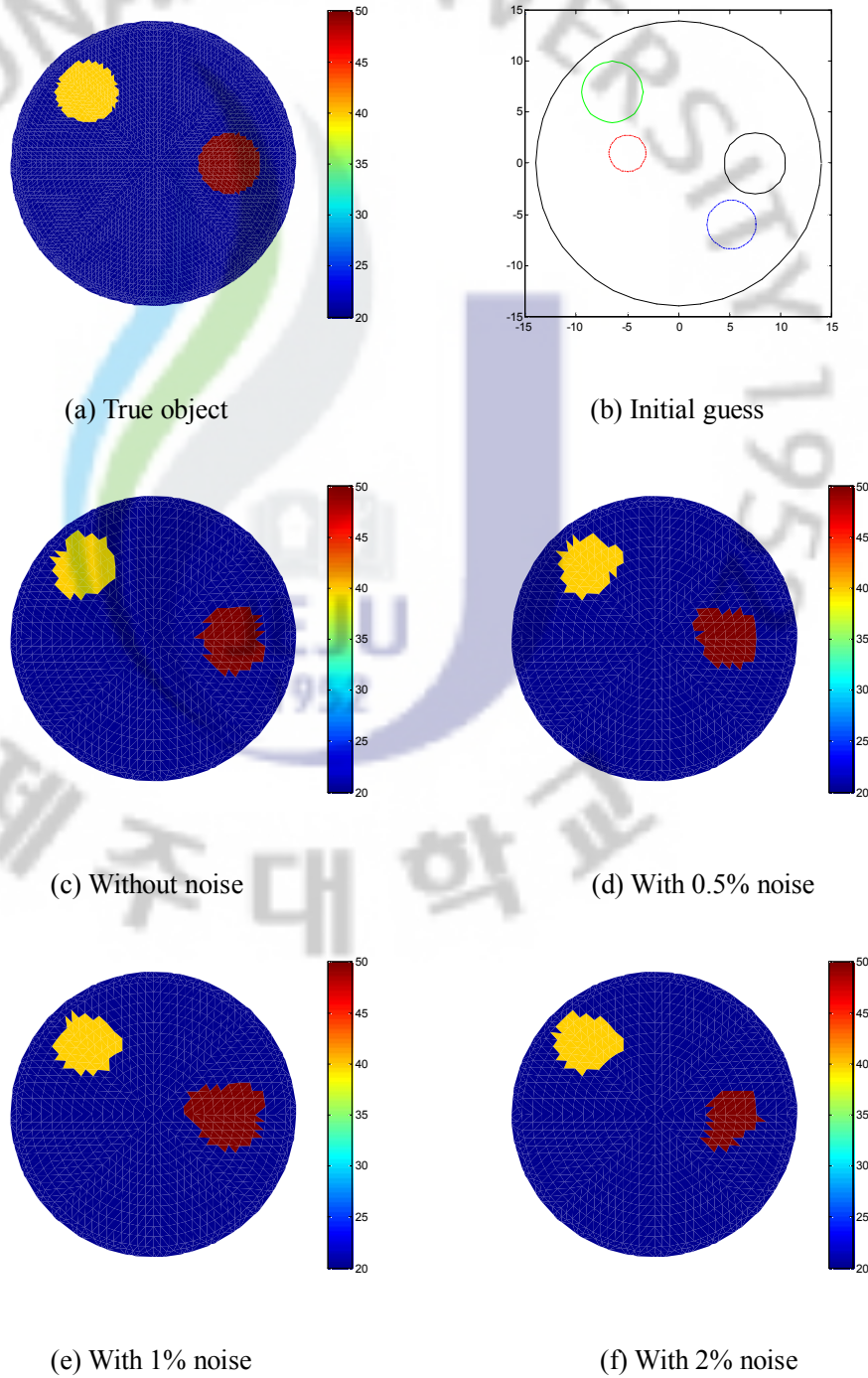
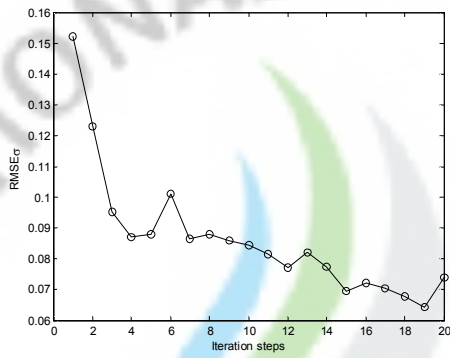
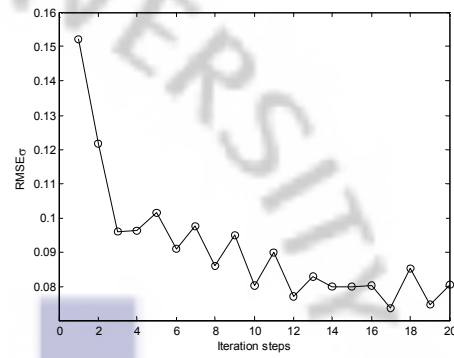


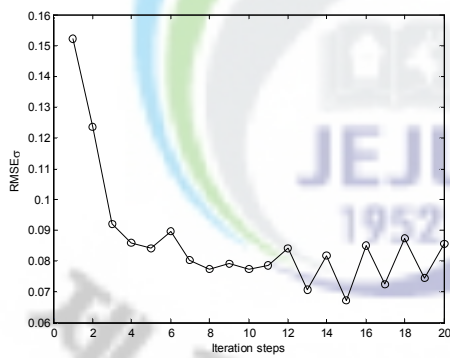
Figure 3.12 True image of resistivity distribution, initial guess (solid line represents the true boundary, while the dashed line shows the initial guess) and final level set reconstruction for case 3 with or without noise.



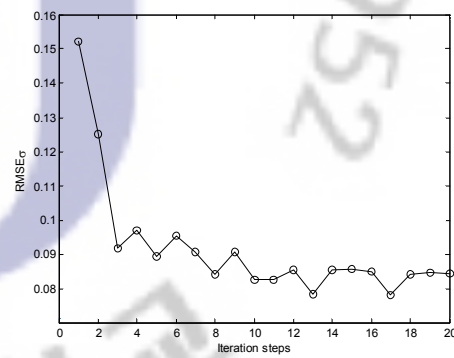
(a) Without noise



(b) With 0.5% noise



(c) With 1% noise



(d) With 2% noise

Figure 3.13 RMSE value of conductivity distribution of case 3 on different noise condition.

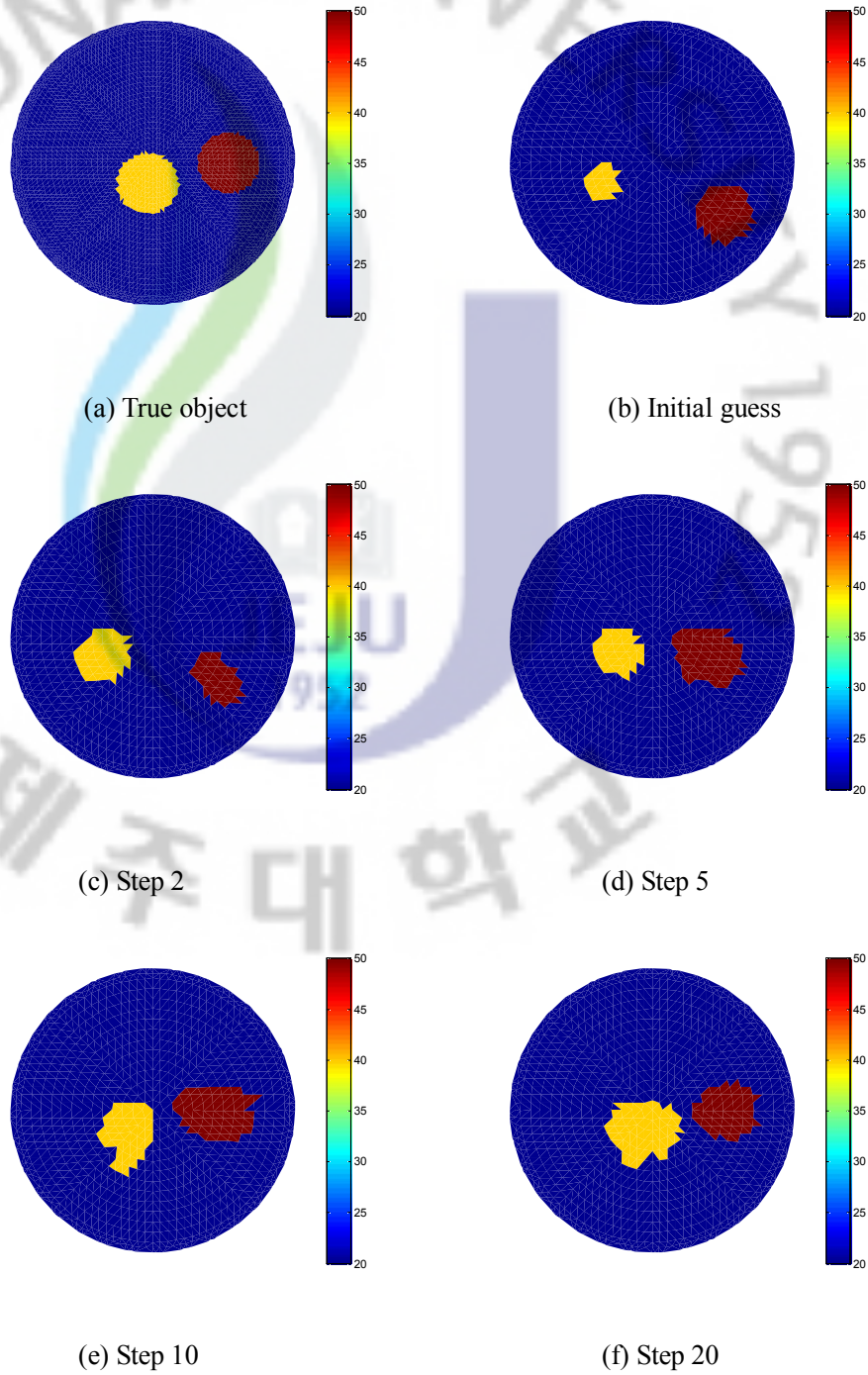


Figure 3.14 True image and evolution of the shape during the level set reconstruction of case 4.

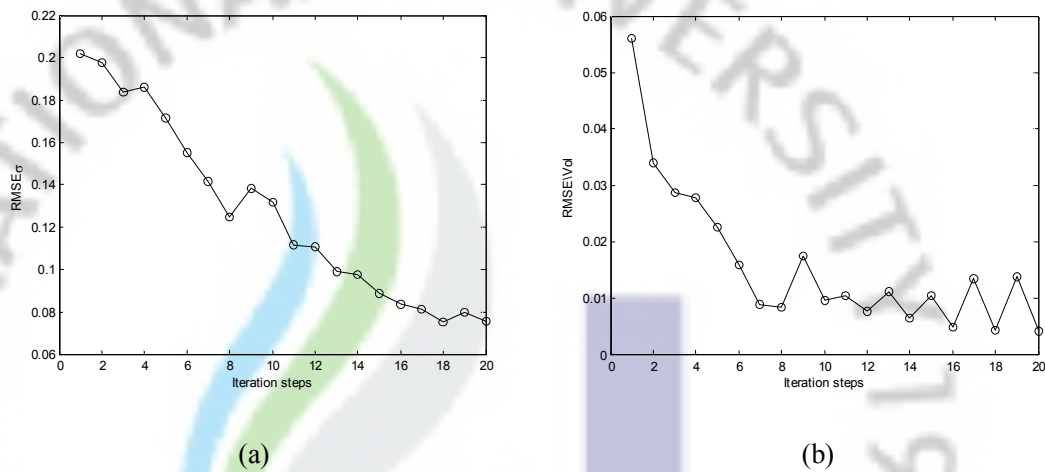


Figure 3.15 Evaluation error of case 4: (a) RMSE value of conductivity distribution and (b) RMSE value of voltage.

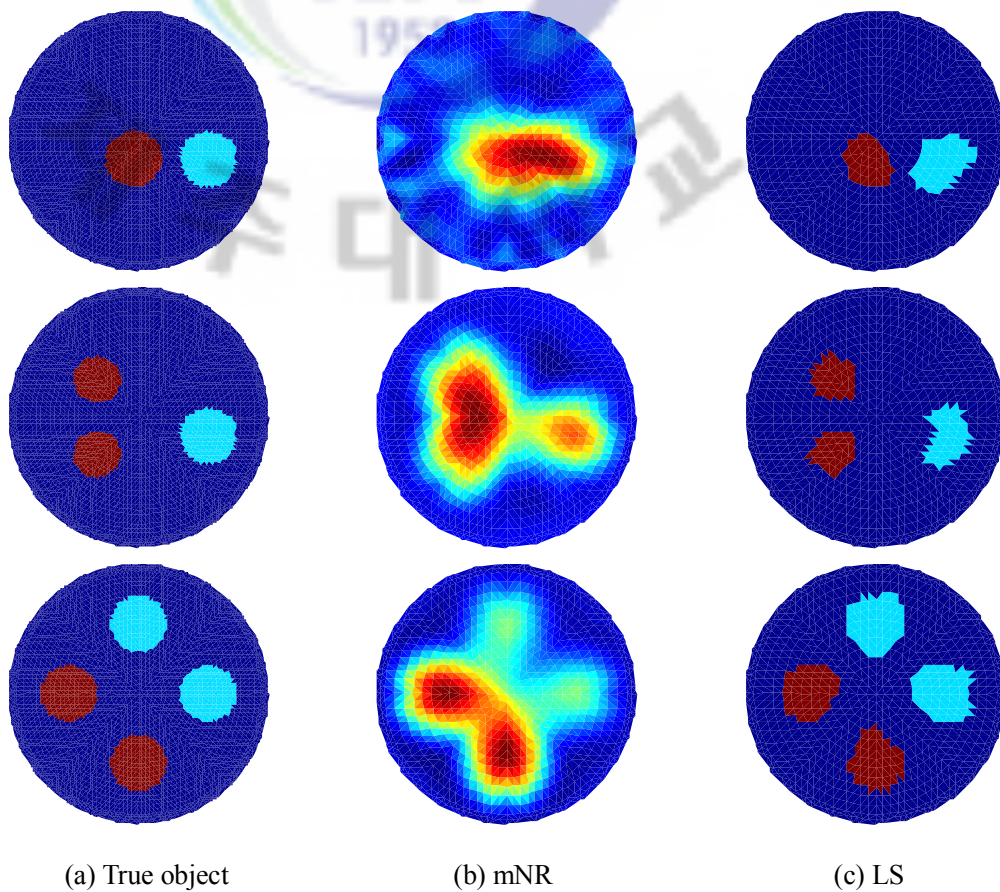


Figure 3.16 Comparison of level set reconstructions and modified Newton-Raphson reconstructions using simulation data. The left column shows the true objects, the central column show the mNR reconstructions and the right column the level set-based reconstructions.

3.3.2 Experimental results

The visualization of multi-phase flow is carried out using the EIT experimental setup in our laboratory (See figure 3.17). The experimental set-up consists a circle phantom with a radius of 140 mm. In order to inject current and measure voltages, 32 stainless steel electrodes, each of 10 mm width and 100 mm height are mounted around the boundary of phantom, as shown in figure 3.17(a). Measurement set-up consists of an Agilent-4284A LCR meter, which is used as a current source and it is connected to an NI PXI-2536 switch module to account for different current patterns. To measure the voltages on the electrodes, the National Instruments PXI-4065 as a $6^{1/2}$ -Digit digital multimeter (DMM) is used that can measure 10 readings/s with higher resolution and up to 3000 readings/s at lower resolutions. To evaluate the performance of our proposed level set algorithm one experiment has been investigated. Experiment for two inclusions is performed using gelatin (4mS/cm) and plastic rods made of acryl, which has infinite conductivity are used as voids in flow field to visualize multi-phase flow conditions, and saline water (11mS/cm) is filled inside the phantom as background. As for the current injection protocol, adjacent current patterns are used. Current of magnitude 10mA is applied across the electrodes and the corresponding voltages are measured. The data obtained is then tested with the level set algorithm. During solving the inverse problem, there is no prior information about the inclusion location, shape and size of the void. Multi-phase conductivity distributions are piecewise constant and the values are *a priori* known. Also, mesh with 3424 triangular elements and 1777 nodes is used for testing the experimental data, see figure 3.18.

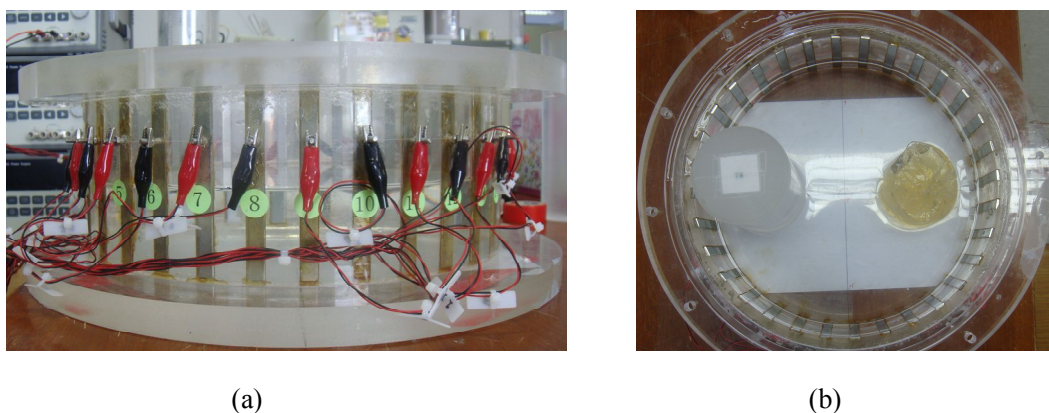


Figure 3.17 EIT measurement system used for multi-phase flow visualization: (a) phantom used for experiment and (b) plastic rod and cylinder gelatin placed inside used as targets

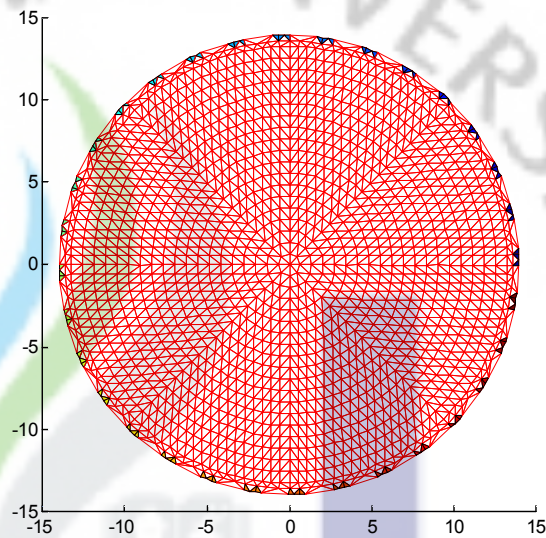


Figure 3.18 FEM mesh used in experimental case

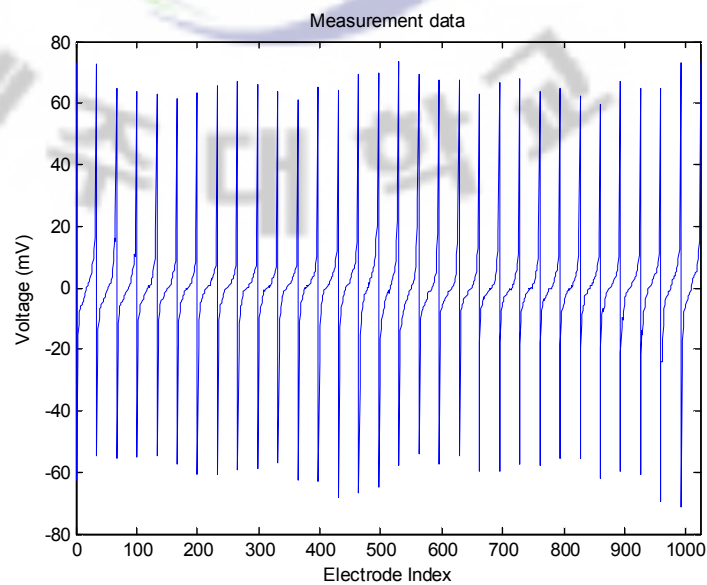


Figure 3.19 Plot of voltage measurements. There are altogether 1024 voltage measurements for 32 electrodes configuration.

Figure 3.19 shows the experimental data collected from a test example from figure 3.17(b). In this test example, the plastic rod and cylinder gelatin are put inside the phantom as the targets. With the injection of adjacent current, 1024 measurement data are taken and used in the reconstruction.

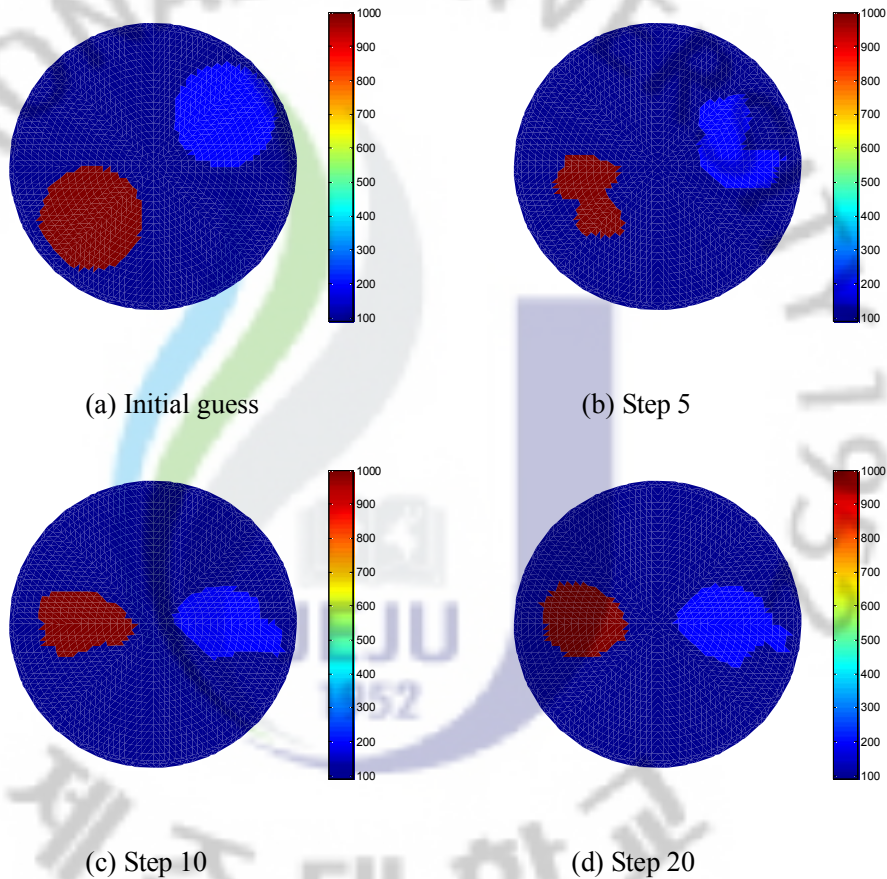


Figure 3.20 Initial guess and the evolution of the shape during the level set reconstruction.

Figure 3.20 shows the evolution of the reconstructed image for the experimental case study using level set method. The initial guess are two circles in the far from the true targets, see figure 3.20 (a). With a choice of the regularization parameter to be $\alpha_1 = 0.1$ and $\alpha_2 = 0.3$, the inclusions can be reconstructed effectively after 20 iterations, also the position and a relatively accuracy of the shape of the inclusions were able to be identified. Figure 3.21 shows the evolution of the RMSE of the voltage during the shape reconstruction process. The result of shape reconstruction using level set-based method shows that this method has a robust solution of multi-phase flow imaging.

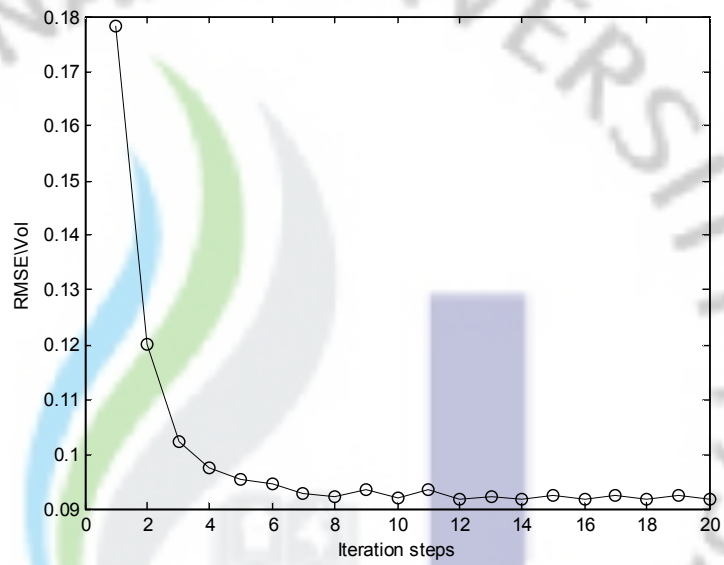


Figure 3.21 RMSE of the voltage during the shape reconstruction process.

4. Conclusions

In this study, electrical impedance tomography is applied to monitor the conductivity or resistivity distribution in an application of multi-phase flow in process tomography. Under the assumption that multi-phase conductivity distributions are piecewise constant and the values are known *a priori*, but the size, topology and shapes of the obstacles are unknown and have to be recovered from the boundary measurement data. The inverse shape reconstruction problem is to find a level set function (which can present a conductivity distribution) that minimizes the mismatch between measured and calculated data. For a shape-based inversion scheme, the unknown shapes can be represented by level set functions which are moving in order to reduce the misfit errors.

Compared to the more typical pixel-based reconstruction methods, the shape-based reconstruction approach has the advantage that the prior information about the high contrast of the inclusions is incorporated explicitly in the modeling of the problem. In a pixel-based reconstruction scheme, such as mNR can be applied to find quickly a good initial guess for the shape evolution, the approximate locations of the unknown inclusions are found easily during the early iterations of the scheme, but it takes a large number of additional iterations in order to actually build up this high contrast to the background due to the smoothing effect of most regularization schemes. Instead, by using the level set-based technique, convergence is extremely fast and very good results are achieved. In case the inclusions are close to each other, pixel-based reconstruction method is hard to separate them clearly, but the proposed scheme is able to successfully separate two nearby objects from each other and also can reconstruct the targets with a high contrast to the background with rather robust solutions. Moreover, this holds true even in situations where having more than two obstacles in the object to be imaged. In an analogous fashion, multiple level set methods can be used to solve more phases and 3D EIT problems.

Summary

In electrical impedance tomography (EIT), an image of the conductivity or permittivity of part of the object is inferred from surface electrical measurements. Typically, conducting electrodes are attached around the object and small alternating currents are applied to some or all of the electrodes. The resulting electrical potentials are measured, and the process may be repeated for numerous different configurations of applied current. Using the measurement voltage, an approximation for the conductivity or resistivity distribution within the object can be obtained. Mathematically, the EIT problem is a nonlinear and ill-posed inverse problem.

In this thesis, a shape reconstruction scheme in EIT for multi-phase flow based on level set methods is studied. The key feature of the scheme is using narrow band level set method to solve the inverse problem of finding the interface between the regions having different conductivity values. In using a multi-phase level set model, the conductivity can be presented by two level set functions. Based on the level set theory, the key idea is to implicitly represent the shape interface as the zero level set of a higher dimensional function and then solve a set of partial differential equations. The level set-based scheme offers several advantages compared to traditional pixel-based approach. The level set strategy handles topological merging and breaking naturally during the evolution process. Extension of level set method for multi-phase case has been presented and tested with several of numerical and experiment data, it is found that shape-based level set method has better reconstruction performance when compared to pixel-based image method.

References

- A. Tamburrino, G. Rubinacci, M. Soleimani, W.R.B. Lionheart. A Noniterative Inversion Method for Electrical Resistance, Capacitance and Inductance Tomography for Two-phase Materials. *Proc. 3rd World Congress on Industrial Process Tomography*, Banff, Canada, pp.233-238, 2003.
- B.H. Brown, A. Leathard, A. Sinton, F.J. McArdle, R.W. Smith, D.C. Barber. Blood flow imaging using electrical impedance tomography. *Clin Phys Physiol Meas*, vol.13, pp.175-179, 1992.
- B.H. Doerstling. A 3-D reconstruction algorithm for the linearized inverse boundary value problem for Maxwell's equations. PhD thesis, Rensselaer Polytechnic Institute, Troy, New York. 1995.
- B. Martin. A level set method for inverse problems. *Inverse problems*, 17:1327-1355, 2001.
- D.C. Barber and B.H. Brown. Applied Potential tomography. *J phys. E: Sci Instrum*, 17:723-733, 1984.
- D.C. Gisser, D. Isaacson and J.C. Newell. Theory and performance of adaptive current tomography system. *Clinical Physics and Physiological Meas*, 9:35-42, 1988.
- D. Isaacson and M. Cheney. Current Problems in Impedance Imaging, with D. Isaacson, *Inverse Problems in Partial Differential Equations*, ed. D. Colton, R. Ewing, and W. Rundell. chapter 9: 141-149, SIAM, Philadelphia, 1990.
- E.T. Chung, T.F. Chan, X.C. Tai. Electrical Impedance Tomography Using Level Set Representation and Total Variational Regularization. *Journal of Computational Physics*, 205: 357-372, 2005.
- E. Somersalo, D. Isaacson and M. Cheney. A linearized inverse boundary value problem for

- Maxwell equations. *J comput. Appl. Math*, 42:123-136, 1992.
- F. Dong , Z. X. Jiang , X. T. Qiao and L. A. Xu. Application of electrical resistance tomography to two-phase pipe flow parameters measurement. *Flow Meas. Instrum*, vol.14:183-192, 2003.
- G.F. Lynch and S.L. Segal, Direct measurement of the void fraction of a two-phase fluid by nuclear magnetic resonance. *International Journal of mass transfer*; 20:7–14, 1977.
- H. Jain, D. Isaacson, P.M. Edic and J.C. Newell. Electrical impedance tomography of complex conductivity distributions with noncircular boundary. *IEEE Trans. Biomed. Eng*, 44:1051-1060, 1997.
- H.J. Jeon, J.H. Kim, B.Y. Choi, K.Y. Kim, M.C. Kim, and S. Kim. Electrical Impedance Imaging of Binary Mixtures with Boundary Estimation Approach Based on Multilayer Neural Network. *IEEE Sensors Journal*, 5(2) 313-319, 2005.
- H.X.Wang, C. Wang, and W.L. Yin. A Pre-Iteration Method for the Inverse Problem in Electrical Impedance Tomography. *IEEE Transactions On Instrumentation And Measurement*, Vol. 53:1093-1096, 2004.
- J. Bond, J. C. Cullivanu, N. Climpson, I. Faulkes, X. Jia, J. A. Kostuch, D. Payton, M. Wang, S. J. Wang, R. M. West, R. A. Williams. Industrial monitoring of hydrocyclone operation using electrical resistance tomography. *Proceedings of 1st World Congress on Industrial Process Tomography*, Buxton, UK. 102–107, 1999.
- J. Couthard, Y. Yan, Ultrasonic cross-correlation flowmeter, *Measurement and Control*, 26, 1993.
- J. Malmivuo and R. Plonsey. Bioelectromagnetism. Oxford university press New York, 1995.
- K. Ito, K. Kunisch, Z. Li. Level set function approach to an inverse interface problem. *Inverse*

Probl, 17:1225-1242, 2001.

K.S. Cheng, D. Isaacson, J.C. Newell, and D.G. Gisser. Electrode models for electric current computed tomography. *IEEE Trans Biomed Eng*, 36:918-924, 1989.

K.Y. Kim, B.S. Kim, M.C. Kim, Y.J. Lee and M. Vauhkonen. Image reconstruction in time varying electrical impedance tomography based on the extended Kalman filter. *Meas. Sci. Technol*, 12:1032-1039, 2001.

L.A. Vese, T.F. Chan. A Multi-phase Level Set Framework for Image Segmentation Using the Mumford and Shah Model. *International Journal of Computer Vision*, Vol. 50(3), 271-293, 2002.

L. E. Baker. Principles of the impedance technique. *IEEE Eng. Med. Biol. Mag.* 8:11-15, 1989.

M. Soleimani, W.R.B. Lionheart, and O. Dorn. Level set reconstruction of conductivity and permittivity from boundary electrical measurements using experimental data. *Inverse Problems in Science and Engineering*, 14:193-210, 2006.

M. Soleimani, O. Dorn, W.R.B. Lionheart. A narrow-band level set method applied to EIT in brain for cryosurgery monitoring. *IEEE Transactions on Biomedical Engineering*, 53(11), 2257-2264, 2006.

M. Vauhkonen. Electrical impedance tomography and prior information, PhD Thesis, University of Kuopio, Finland. 1997.

M. Wang, A. Dorward, D. Vlaey, R. Mann, Measurements of gas-liquid mixing in a stirred vessel using electrical resistance tomography (ERT). *Proceedings of 1st World Congress on Industrial Process Tomography*, Buxton, UK, 78-83, 1999.

N. Polydorides and W.R.B. Lionheart. A MATLAB toolkit for three-dimensional electrical

impedance tomography: A contribution to the electrical impedance and diffuse optical reconstruction software project. *Meas. Sci. Technol.*, 13:1871-1883, 2002.

O. Dorn, E. M. Miller, and C. M. Rappaport. A shape reconstruction method for electrono-magnetic tomography using adjoint and level sets. *Inverse problems*, 16:1119–1156, 2000.

O. Dorn, D. Lesselier. Topic Review: Level set methods for inverse scattering. *Inverse problems*, 22:67-131, 2006.

P. Ola, L. Paivarinta and E. Sommersalo. An inverse boundary value problem in electrodynamics. *Duke Math J*, 70:617-653, 1993.

R. Halter, A. Hartov and K. Paulsen. Video rate electrical impedance tomography of vascular changes: preclinical development. *Physiol. Meas.*, 29:349-364, 2008.

R.A. Kumar, R.L. Cook, O.P. Norton, W.O. Okhaysen. Laser based cross-correlation technique for the determination of flow velocities in multi-phase flows. *Proceedings of 1st International Symposium on Measurement Techniques for Multi-phase Flows*, Nanjing, PR China, 386–398. 1995.

S. Banerjee and R.T. Lahey. Advances in two-phase flow instrumentation. *Advances Nuclear Science Technology*, 13: 227–414, 1981

S. Osher and R. P. Fedkiw. Level set methods: an overview and some recent results. *J.Comput. Phys*, 169(2):463–502, 2001.

S. Osher and R. Fedkiw. Level set methods and dynamic implicit surfaces, volume 153 of Applied Mathematical Sciences. Springer-Verlag, New York, 2003.

S. Osher and J.A. Sethian. Fronts propagating with curvature-dependent speed: algorithms based

on Hamilton-Jacobi formulations. *J. Comput. Phys*, 79, 12–49, 1988.

T.E. Kerner, A. Hartov, S.K. Soho, S.P. Poplack and K.D. Paulsen. Imaging the breast with IS: an initial study of exam consistency. *Physiol. Meas*, 23:221–36, 2002.

V.A. Cherepenin, A.Y. Karpov, A.V. Korjnevsky, V.N. Kornienko, Y.S. Kultiasov, M.B. Ochapkin, O. V. Trochanova, and J. D. Meister. Three-dimensional EIT imaging of breast tissues: System design and clinical testing. *IEEE Trans. Med. Imag*, 21 662–667, 2002

V. Cherepenin, A. Karpov, A. Korjnevsky, V. Kornienko, A. Mazaletskaya and D. Mazourov. A 3D electrical impedance tomography (EIT) system for breast cancer detection. *Physiol. Meas*, 22 9–18, 2001.

V. Kolehmainen, S.R. Arridge, W.R.B. Lionheart, M. Vauhkonen, J. P. Kaipio. Recovery Of Region Boundaries Of Piecewise Constant Coefficients Of An Elliptic PDE From Boundary Data. *Inverse problems*, 15:1375-1391, 1999.

Y. Li, L.Y. Rao, R.J. He, G.Z. Xu, X. Guo, W. L. Yan, L. Wang, and S. Yang. Three EIT Approaches for Static Imaging of Head. *Conf Proc IEEE Eng Med Biol Soc*. 1:578-81, 2004.